

Advanced Microscopy Course 2012

Lecture 5: Basic Image Processing

Lecture 16: Applied Image Processing
Graeme Ball

Richard Parton - Richard.Parton@bioch.ox.ac.uk
Department of Biochemistry
University of Oxford

Basic Image Processing

- What is a digital image?
- What makes a good image?
 - Correct image acquisition
 - Signal to Noise
 - Resolution and Sampling
- The basics of image processing
 - Golden rules of image processing
 - Conceptual Hierarchy of Image Processing
 - Low Level Processing:
 - Display
 - Filtering
 - Mid - Level Processing:
 - Segmentation
 - Spectral unmixing
 - High -Level Processing:
 - Colocalisation
 - Tracking
 - Statistics

What is a digital image?

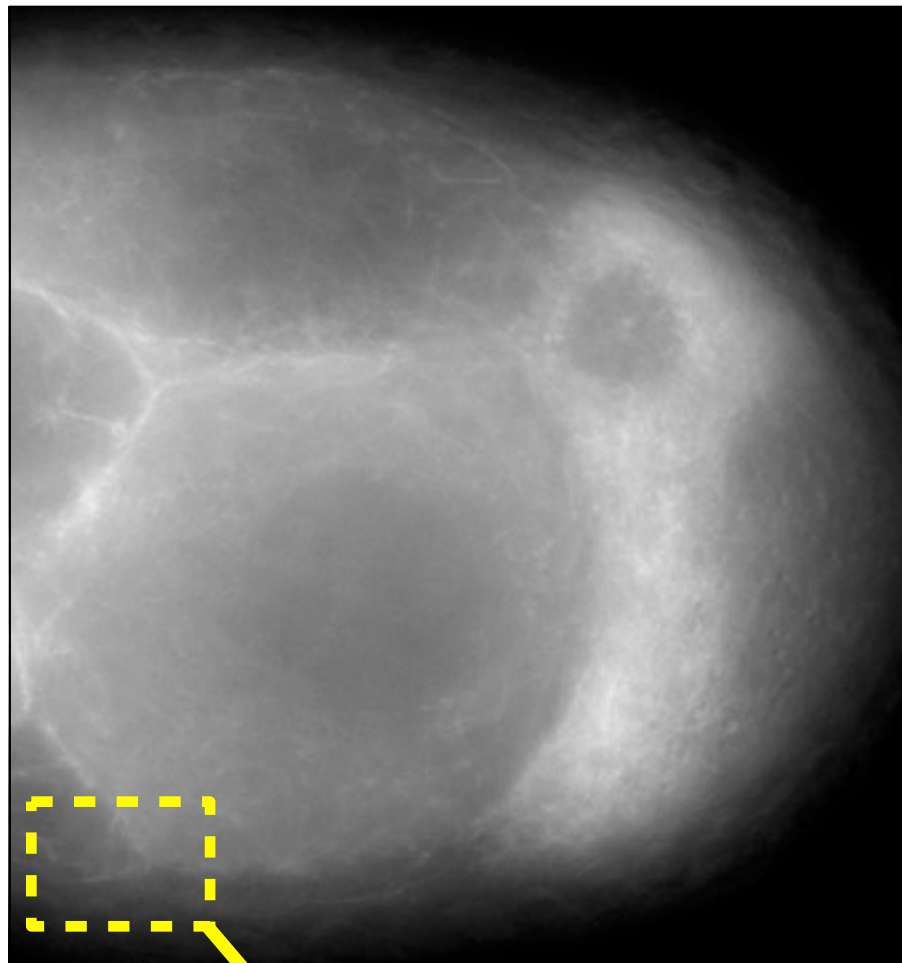


What is a digital image?

An image represents the output of the optics and detector of the imaging system

image $\neq$ object

image = object $\otimes$ PSF



258	544	1193	1969	2370	2063	1301	613	263
286	562	1173	1893	2251	1959	1241	596	278
313	585	1129	1760	2073	1791	1156	577	300
365	622	1000	1407	1630	1378	930	514	357
386	629	916	1215	1388	1154	819	491	373
401	613	819	1026	1148	946	709	467	372
411	526	613	678	784	614	518	420	328
406	477	511	523	589	458	425	387	307
387	419	420	405	364	340	349	345	284
321	327	307	320	268	260	271	261	245
282	267	243	254	202	203	222	215	217
238	216	193	205	163	165	185	177	186

- A digital image is a **numerical array**: elements = **pixels** or **voxels** with:
 - **defined size** (sampling resolution)
 - defined no. of **grey levels** (bit depth)
- In addition to “useful” signal there is:
 - **dark signal** from the detector
 - **autofluorescence** (background)
 - **statistical noise** of photon detection
- Details are detected within the limitations of:
 - the **imaging optics**
 - the **sampling rate** (pixel size)
 - the **statistical noise**
 - the **sample contrast / detector dynamic range**

Image Parameters - what to record (= image metadata)

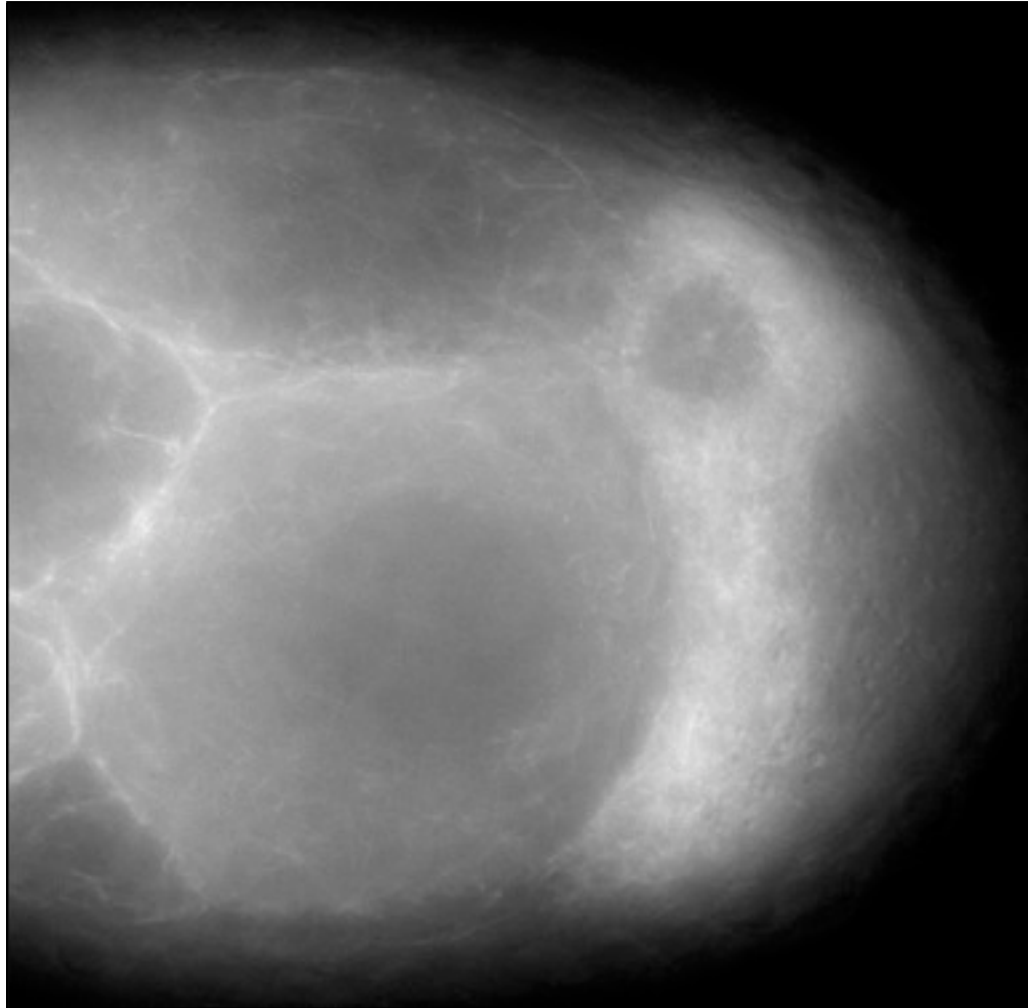
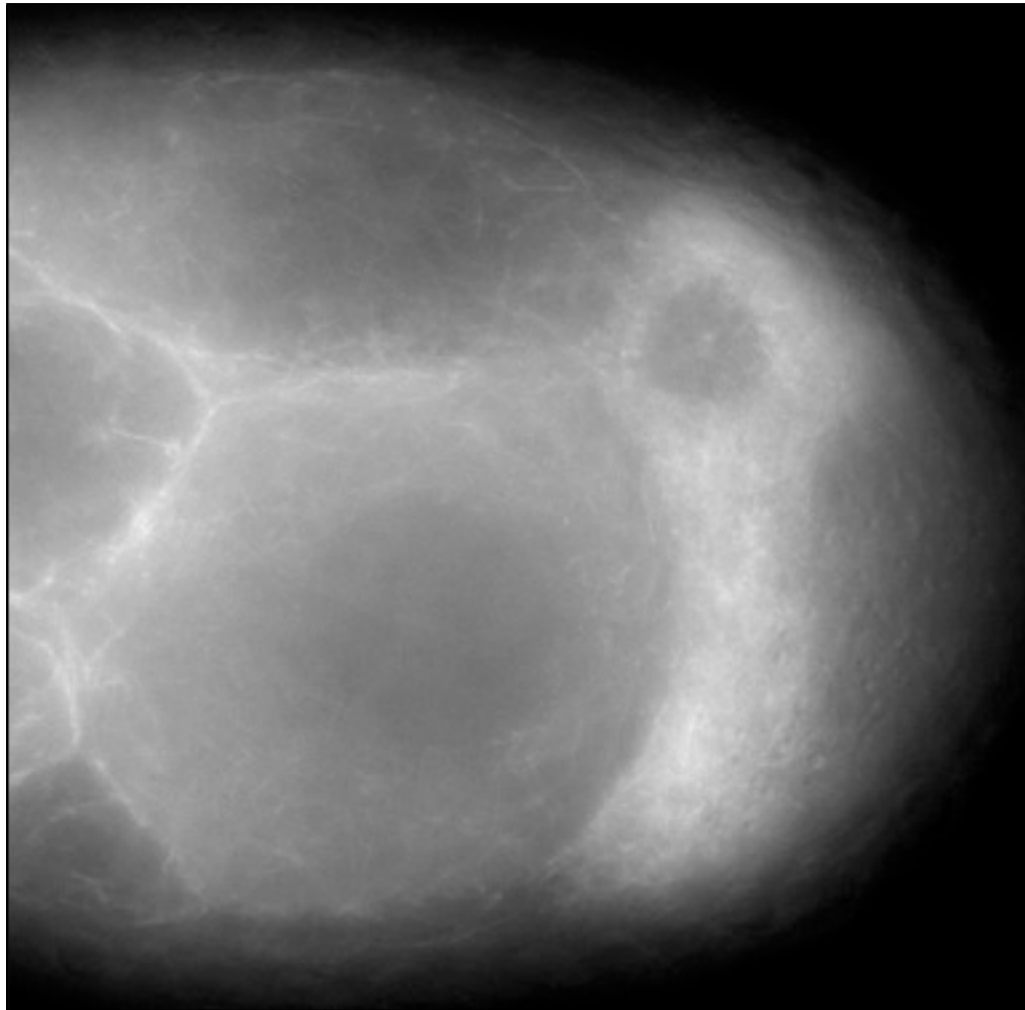


Image Parameters - what to record (= image metadata)



Wide-field fluorescence 490 ex 520 em
X60 1.2 WI
xy 212 nm; 60 (z step 200 nm)
Bin 2x2
250 ms exposure
Contrast stretched to fill 8 bit display
Tau-GFP Oocyte

- **Type of imaging** – Wide-field fluorescence
- **Excitation and Emission** wavelengths 490/520
- **Optics used** – x60 NA 1.2 water immersion
- **Image pixel dimensions** – 212x212 (x200) nm
- **Depth** or Dynamic range – 8 bit; 256 greys
- **Any processing** performed
 - 12 bit to 8 bit conversion
 - contrast adjustment
- **Display parameters** - range 0-255, grey scale
 - gamma = 1
- **The Biology** - Drosophila stage 8 egg chamber
 - Tau GFP, labelling microtubules

What makes a good image?



Correct Image Acquisition

- The system must be correctly set up and **aligned**
 - **PSF** verification (beads)
- The specimen should not cause undue **optical aberration**
 - mounting / appropriate optics
- Avoid **underflow** and **overflow** but fill the **dynamic range**
 - use a **colour LUT**
 - beware of **auto-intensity scaling**
- Take a **dark signal image** and/or **background**
 - Dark subtraction processing
- Be aware of **XYZ optical resolution** of the system and **sample appropriately**
 - **PSF** of the imaging system
 - **Pixel** (voxel in 3D) **size** in the image
- Take care with **signal to noise** limitations
 - collect enough light: **integrate, average**



Noise / Signal to Noise (S/N)



Signal to Noise - definitions:

- One of the **most important limitations** to image quality and image processing

$$\text{S:N ratio} = \frac{\text{Signal}}{\text{Variation in the signal}}$$

$$\frac{\text{mean}}{\text{S.D.}}$$

- Noise is **NOT** background, auto-fluorescence or dark signal
- Good image data has a **high** S:N ratio
- Fundamental limit = Poisson distributed statistics of photon detection (shot noise)

$$\text{Poisson distributed variation} \quad \text{S:N ratio} = \frac{n}{\sqrt{n}}$$

- Statistics of photon counting dictate the **minimum useful signal**

Average signal = 9,	S:N ratio = 3
Average signal = 100,	S:N ratio = 10
Average signal = 10,000,	S:N ratio = 100

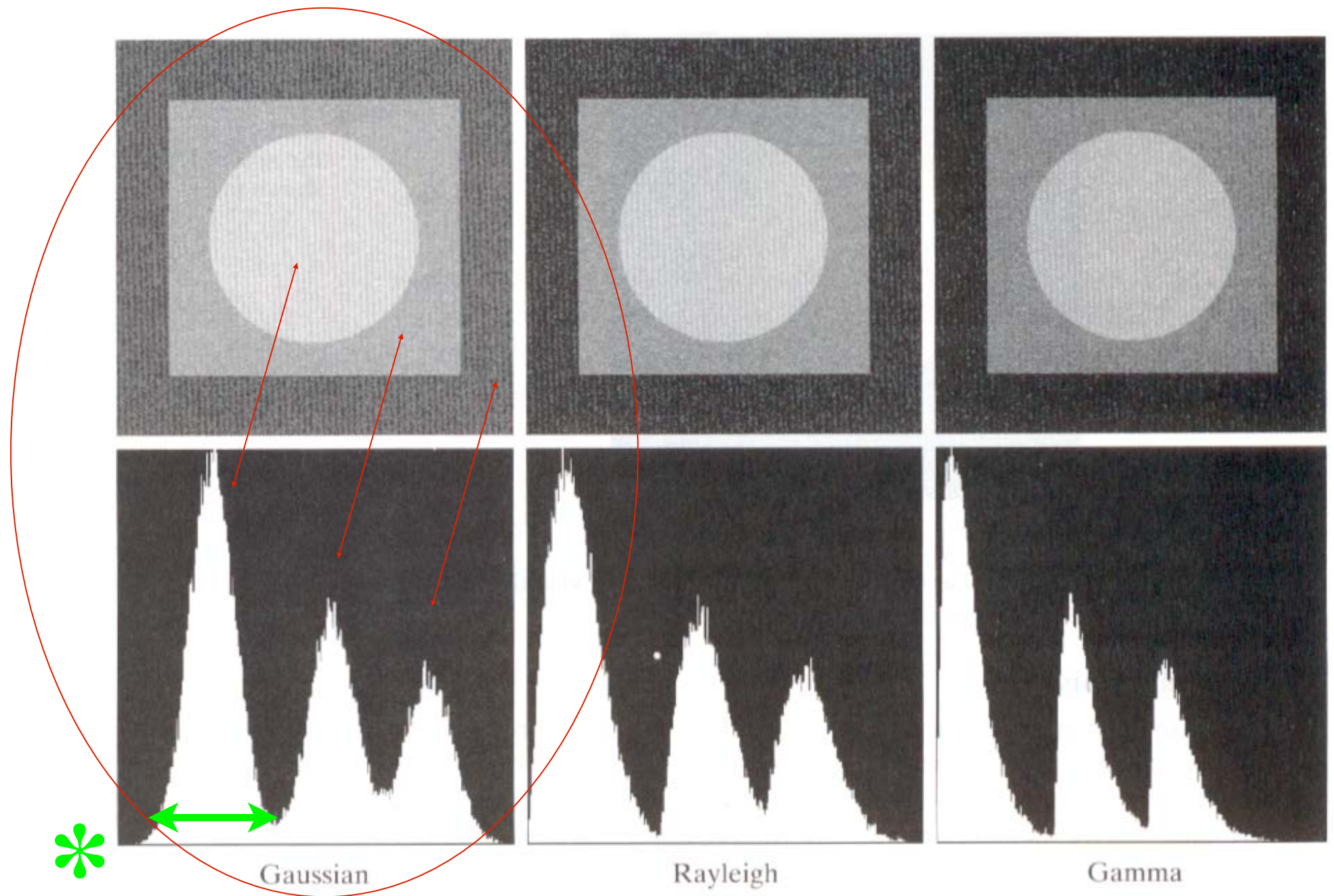
A meaningful difference in intensity
needs to be at least three times the noise level

- Additional sources of noise from **digitisation, detector readout, thermal noise.**

Signal to noise

- noise types

Most commonly used noise model for image processing = **Gaussian**



Avoid propagating noise

- **Noise** is additive:

SO subtracting one noisy image from another propagates noise

THEREFORE

Subtract an **AVERAGE signal** to avoid noise propagation

Or

Where the signal is non-uniform across the field subtract a **4x AVERAGED image** to avoid noise propagation

How to deal with signal to noise

Acquisition

- Use sensitive, high dynamic range, low noise detectors: cooled CCD, EMCCD
- Count as many photons as possible:
 - Bright dyes
 - Good excitation / emission
 - Integration time (accumulation or averaging)

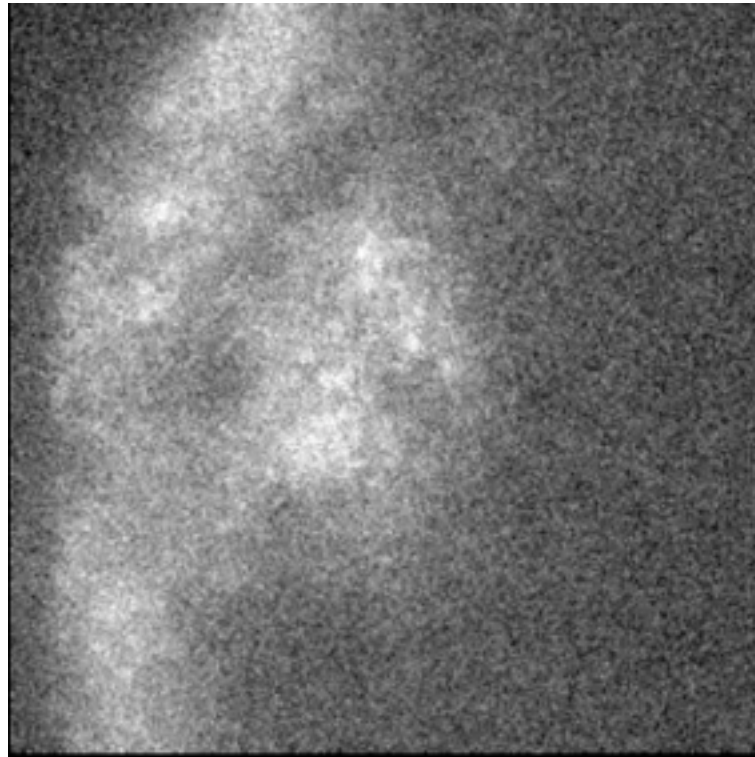
Post Acquisition

- Image averaging
- Noise reduction filtering using a spatial filtering mask – 3x3 median filter
- Noise reduction filtering in the frequency domain – Fourier bandpass filter

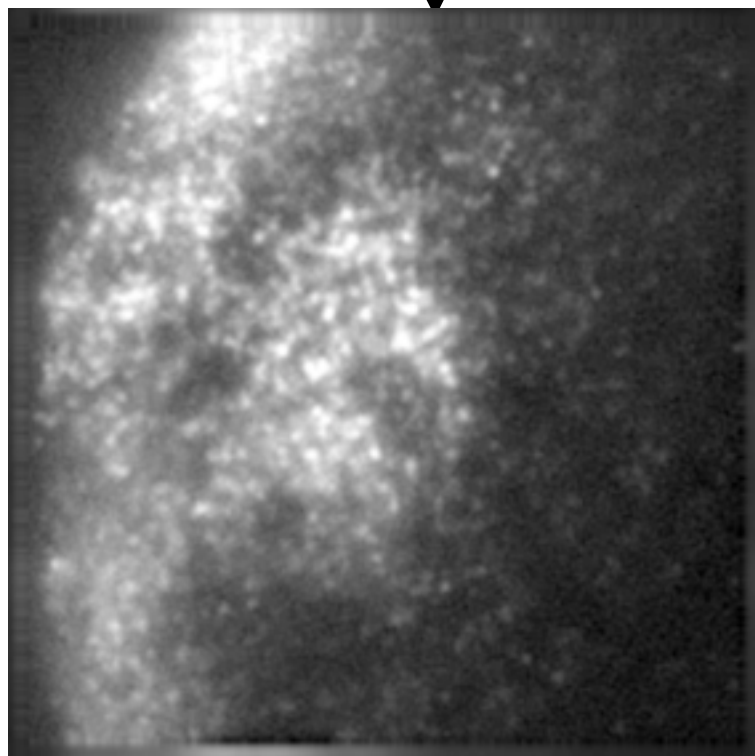
Improving signal to noise

Averaging increases S/N = improved contrast

Single noisy image



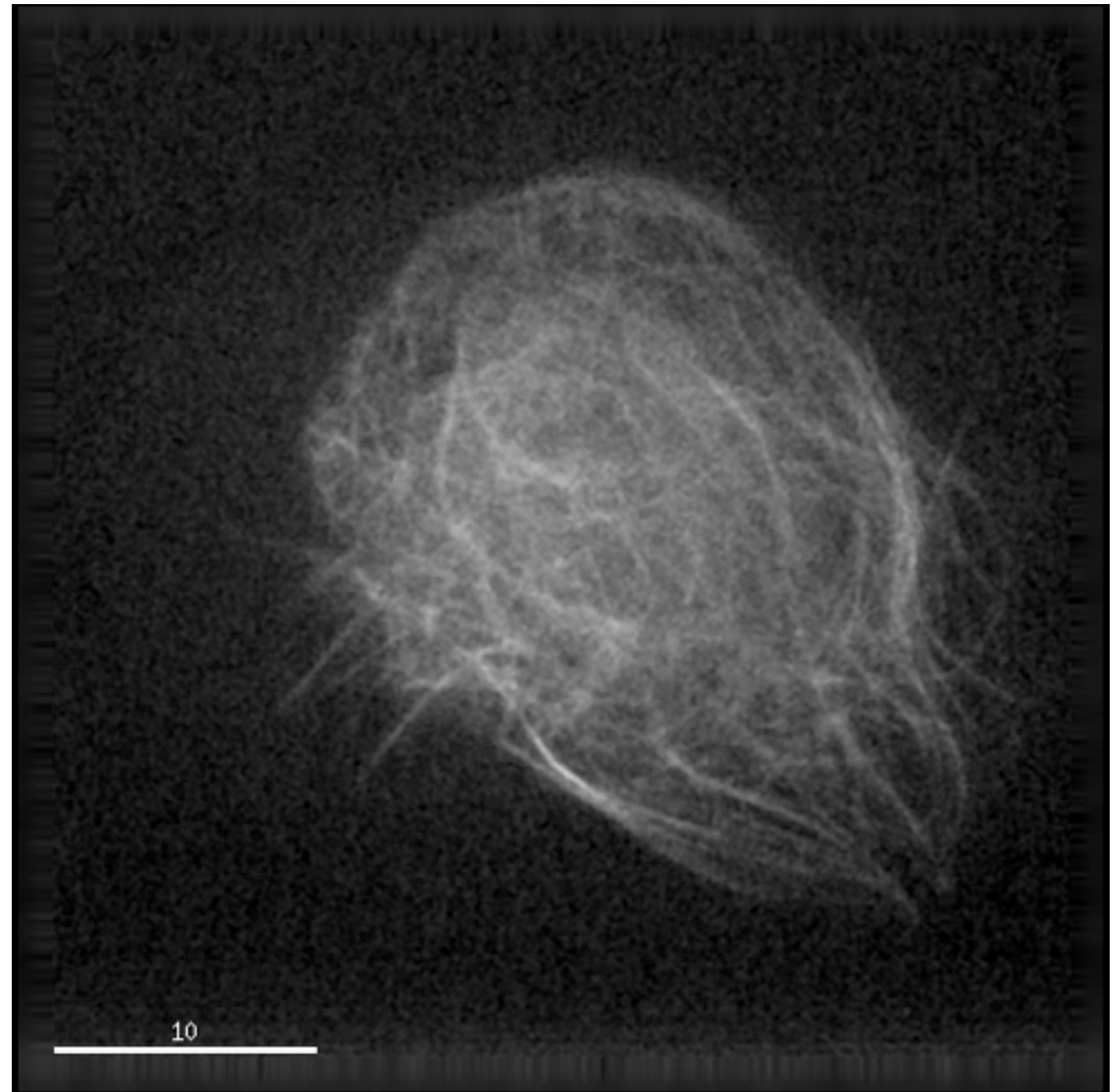
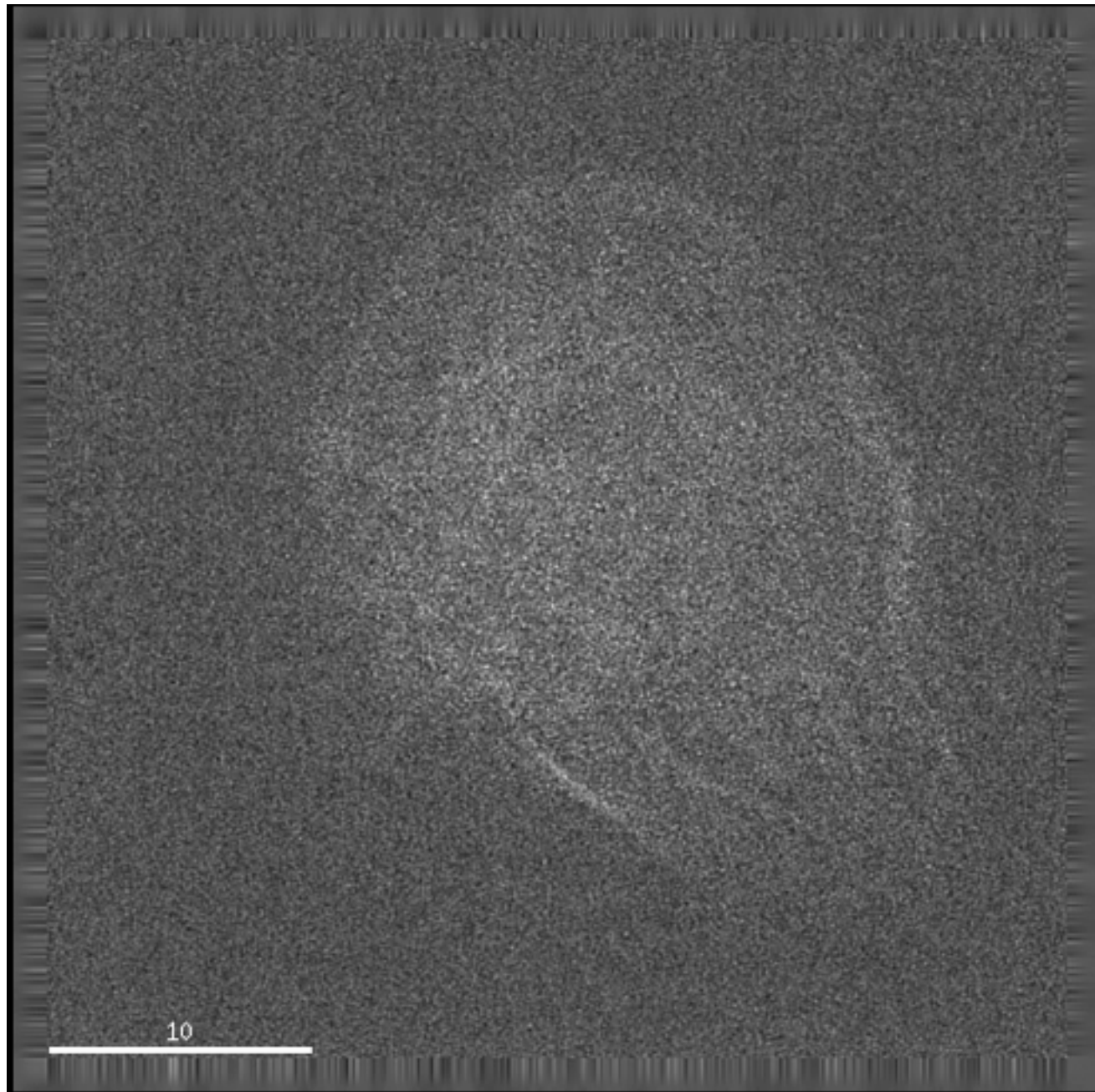
Average 5x successive images ↓



Effectively increases the number of photons counted

improved S/N

Post acquisition denoising



Macrophage: Jupiter-GFP 7Z, 3stacks/s

Jerome Boulanger: SAFIR Denoising software

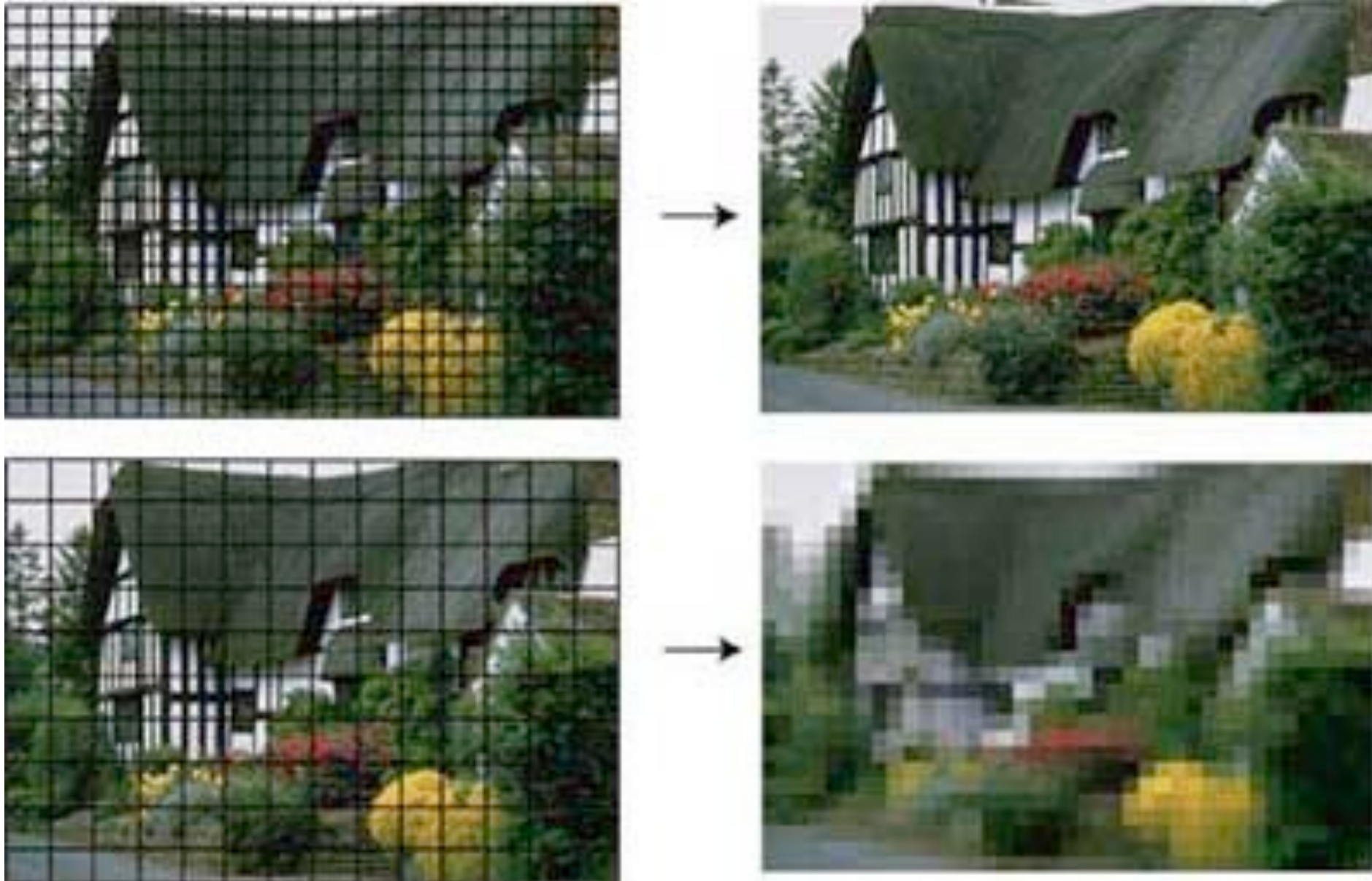
Integrated into Priism by the John Sedat Group UCSF

J. Boulanger, C. Kervrann, and P. Bouthemy, "Space-time adaptation for patch-based image sequence restoration," *IEEE Trans. on Pattern Analysis and Machine Intelligence*, vol. 29, no. 6, pp. 1096–1102, June 2007

Signal to noise - take home messages

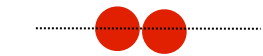
- The definitions of noise components in image data are **confusing**.
- Noise = **VARIATION in signal** - you cannot simply subtract a “noise value”.
- Noise is **NOT** dark signal or background but they **CONTRIBUTE** to image noise.
- Dark signal = generated by camera
 - Has an **average value component** and a **noise (variation) component**.
 - Subtracting a dark offset value does not remove the noise component.
- Background = autofluorescence of sample
 - Is a **real fluorescence signal** and has **associated shot noise**.
 - Subtracting an autofluorescence image does not remove the noise.
- Statistical analysis on intensity should strictly be in relation to **photon counts** (not pixel values).

Resolution and Sampling

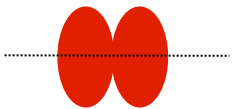


Optical resolution: The Rayleigh Criterion

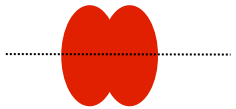
Two small objects



Convolved by microscope



Just
resolved



Not resolved
Airy patterns must
Overlap by less
Than 42% of the
Maximal intensities

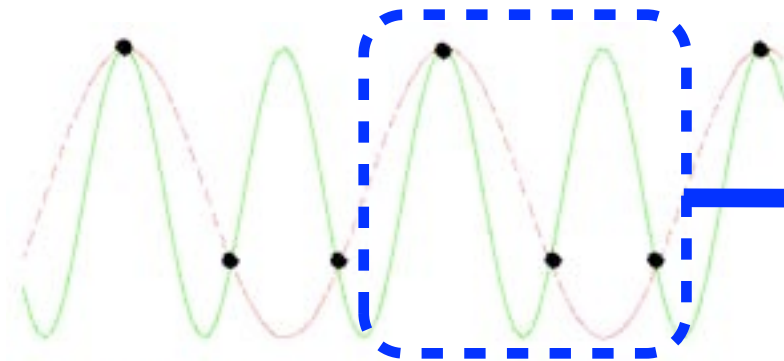
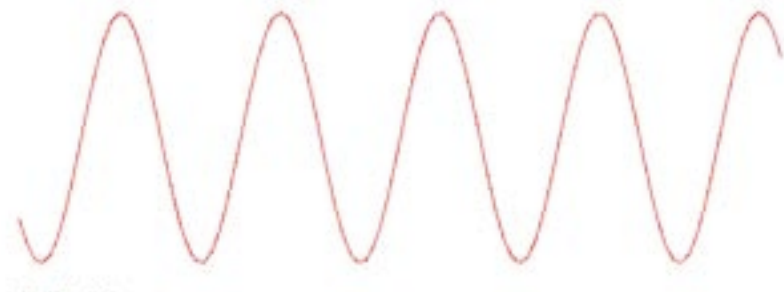
resolution limit $\approx \lambda_{em}/2$

XY resolution ~ 200 nm

Z resolution ~ 500 nm

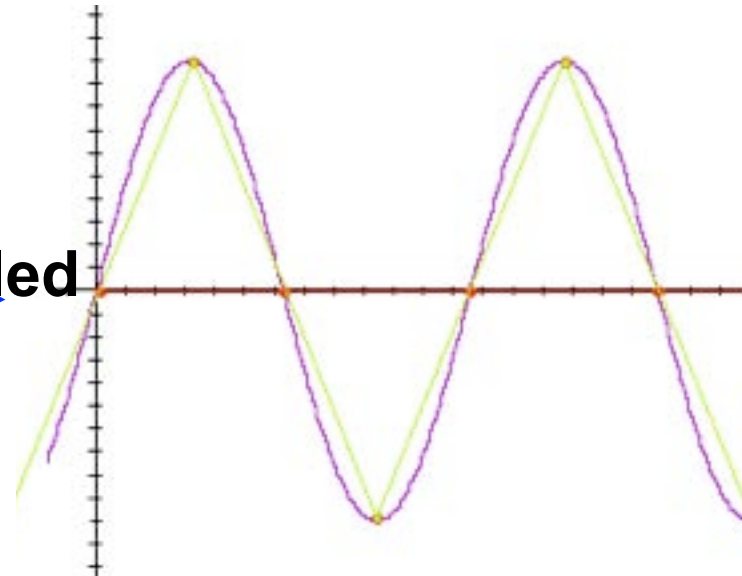
Resolution: Nyquist sampling theorem

A sine wave



Sampling 1.5 times per cycle

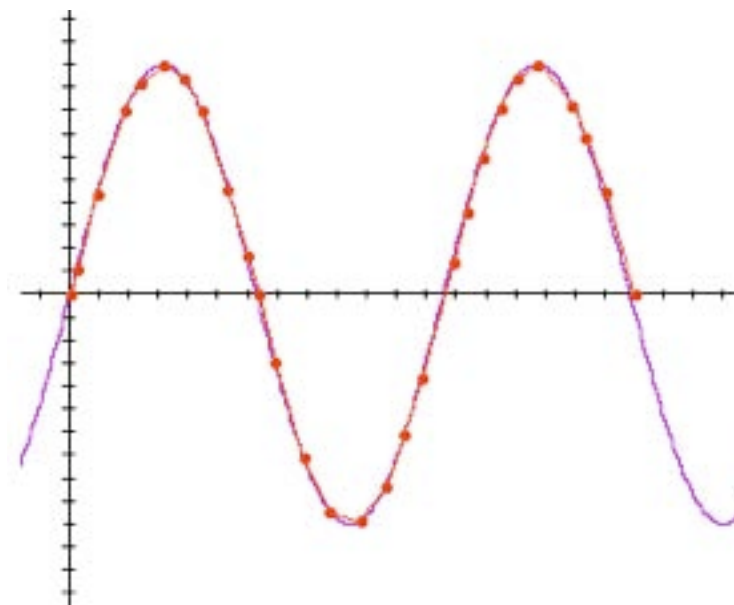
undersampled



Sampling 2.0 times per cycle

just sampled
enough

2.3



Sampling many times per cycle

over sampled

Resolution: sampling

**Theoretical Axial
Resolution (em 525 nm)**

1.4 oil = 229 nm

1.35 oil = 237 nm

1.2 water = 267 nm

0.75 air = 427 nm

**Appropriate Sampling According to Nyquist
theorem - at least half the size**

Nyquist ~ sample at 0.100 um/pixel

Nyquist – sample at 0.103 um/pixel

Nyquist – sample at 0.116 um/pixel

Nyquist – sample at 0.186 um/pixel

**Pixel size on Delta
Vision**

x100 = 0.063 um/pixel

x60 = 0.106 um/pixel

x40 = 0.158 um/pixel

x20 = 0.317 um/pixel

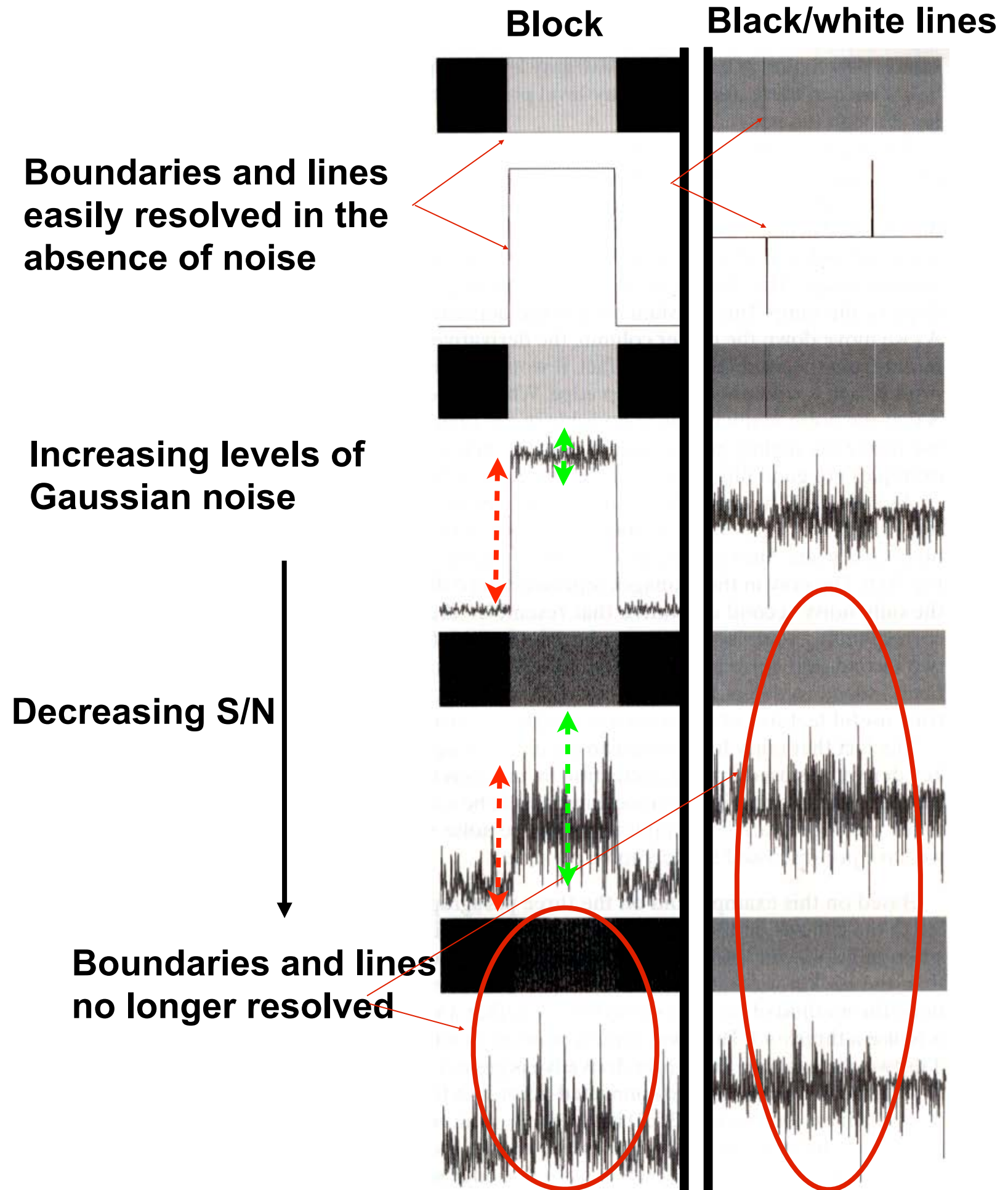
- **Undersampling** limits the data available

Resolution, contrast, noise

- Noise limits the contrast which limits the details that can be resolved
= Noise limits resolution

Resolution, contrast, noise

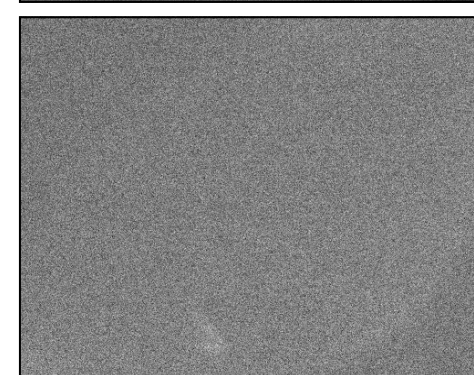
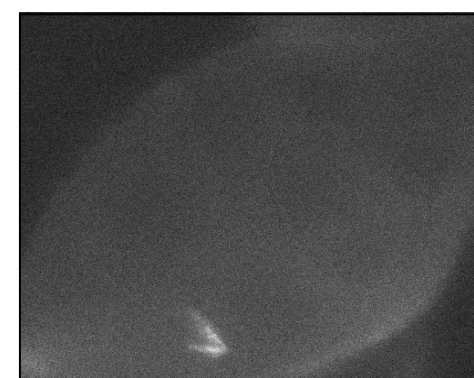
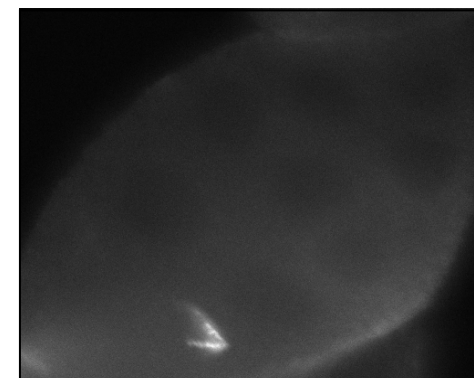
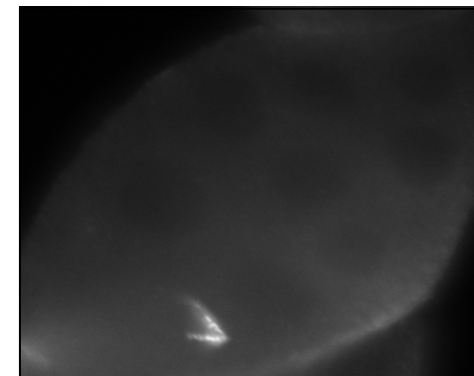
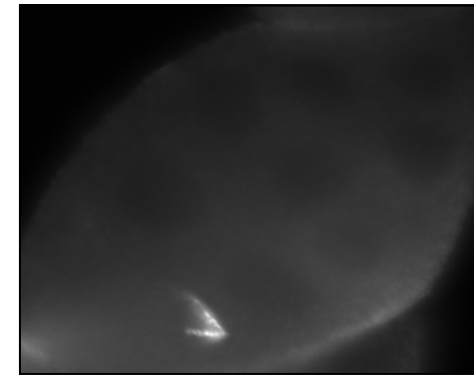
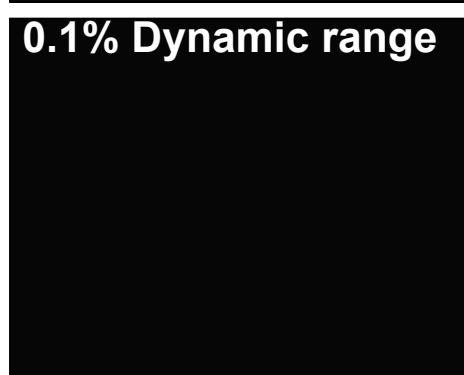
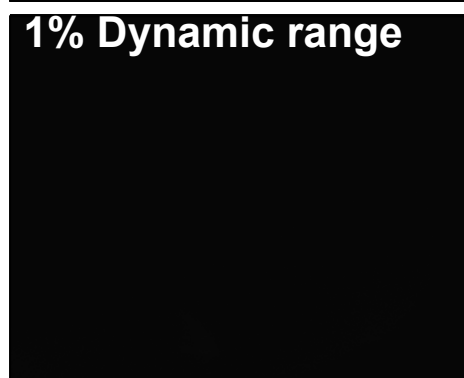
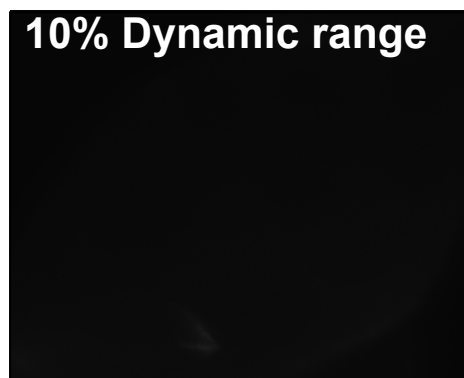
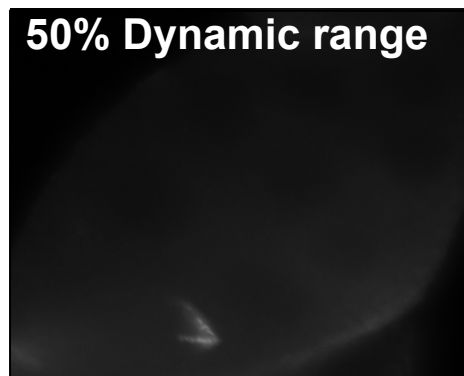
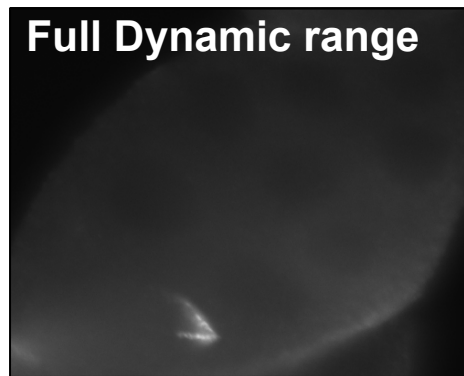
The **difference between signal and background** must be at least 3X the **noise** to be detectable



Resolution Contrast noise

Scaled 0 - 4095

Auto Intensity Scaled display



Decreasing S/N

Increasingly
Noisy looking

Decreasing
Image quality

Cannot resolve

Image series collected by
decreasing the excitation
lamp intensity from 100% to
50%, 10%, 1%, and 0.1%

The basics of image processing



"I want you to make me the fairest
of them all."

Remember what makes a good image

- Good image data has a **high S:N ratio** (count more photons)
- **Correctly sampled** to reproduce the optical resolution
(pixel = resolution/2)
- **Avoid aberrations** (sample prep / choice of objective / technique)
 - spherical aberration (SA)
 - motion blur
 - bad system alignment
- **Correctly annotated** (Metadata retained)

Image Processing is **NOT** a substitute for a good image

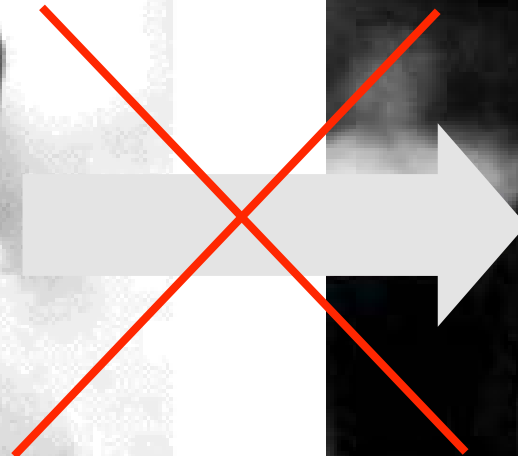
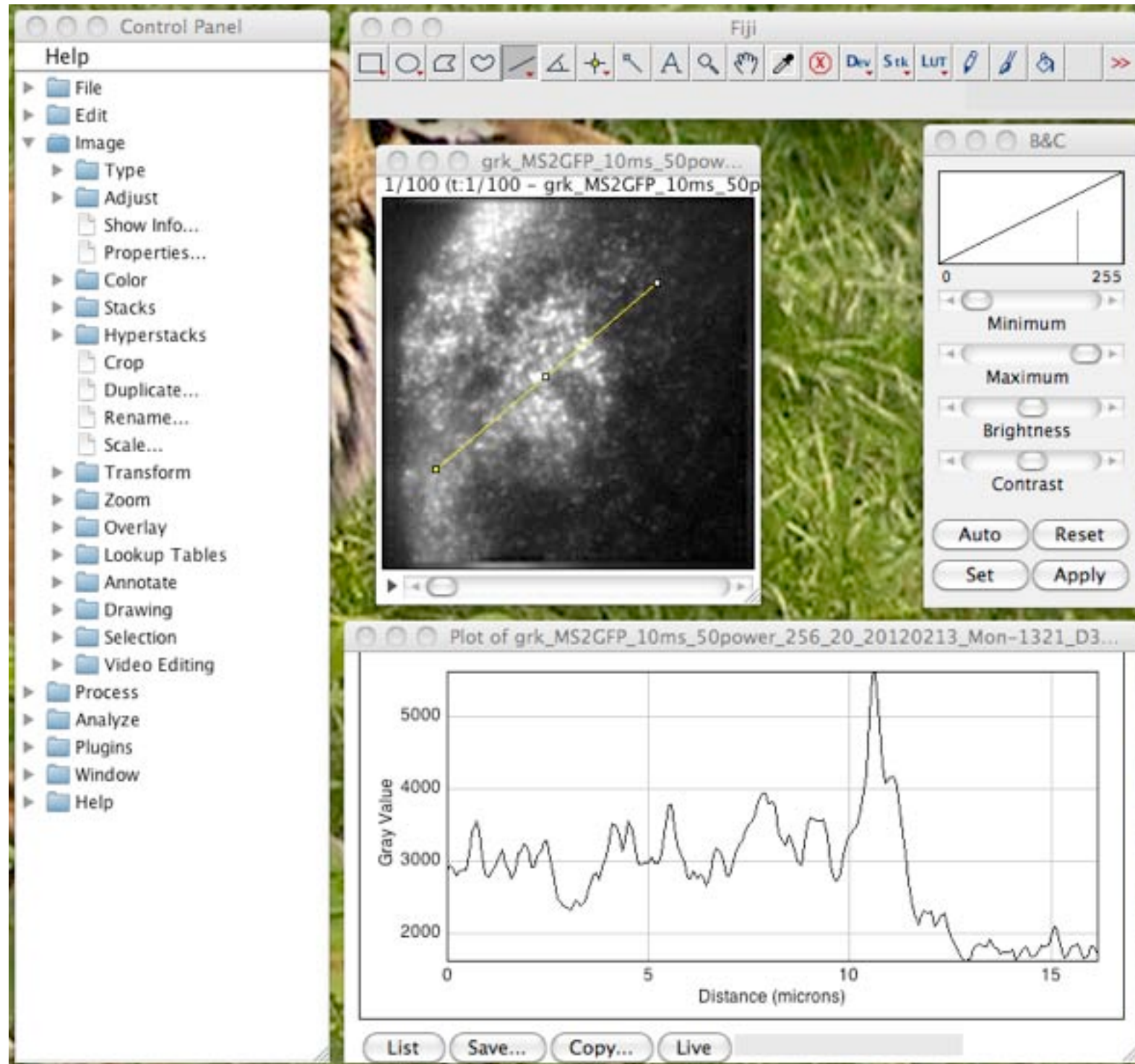


Image J program

<http://rsb.info.nih.gov/ij/>

- Image J is **FREE** and works on MAC, PC and linux
- Consists of a core program and plugins
- Uses Loci Bioformats to convert between file types

<http://loci.wisc.edu/software/bio-formats>



Fiji Is Just ImageJ

<http://fiji.sc/wiki/index.php/Fiji>

For users, Fiji is easy to install and has an automatic update function, bundles a lot of plugins and offers comprehensive documentation.

Golden Rules of Image Processing

- Always **retain the original data**
- **Do not corrupt** the integrity of the original data through processing:
Processing **should NOT generate data** not present in the original image
- Images are **arrays of numerical data** and should be given appropriate consideration.
- Always **record and report all processing steps.**

Preserve your data: File Formats

- In preference use **Uncompressed TIF** (tagged image file format)
- **AVOID** compressed file formats: JPEG, compressed TIF...
This will cause data corruption and loss
- Most data is collected as single channel **grey scale images at 8 or 16 bit depth**
Avoid saving primary image data in colour formats (RGB)
- **Avoid repeated inter-conversions** of file formats
- **Retain your original data in its original file format and original metadata associations**
- Consider **OME file format** for data archiving (lecture 16 - OME, bioformats)
<http://loci.wisc.edu/software/bio-formats>
- Prepare figures for publication in Adobe **Photoshop** in TIFF format and PSD. Arrange and annotate in Adobe **Illustrator**

OME - Open Microscopy Environment



- **Purpose: Supporting Metadata Management for Microscopy**
 - avoids problems of image formats
 - archiving and retrieval
 - data sharing
 - processing
- **A multi-site collaborative effort among academic laboratories and commercial entities:**
 - Dundee - Jason Swedlow**
 - NIA Baltimore - Ilya Goldberg**
 - Harvard Medical School - Peter Sorger**
 - Loci - Kevin Eliceiri**
- **All OME formats and software are FREE**
- **Visit** <http://www.openmicroscopy.org/>
- **We have now set up an OME server associated with MICRON** (Graeme Ball / Ian Dobbie)

Bad Imaging Practices

Do not corrupt the integrity of the
original data

Examples of Bad Imaging Practices

Rossner & Yamada (2004). What's in a picture? The temptation of image manipulation. J. Cell Biology 166: 11–15.

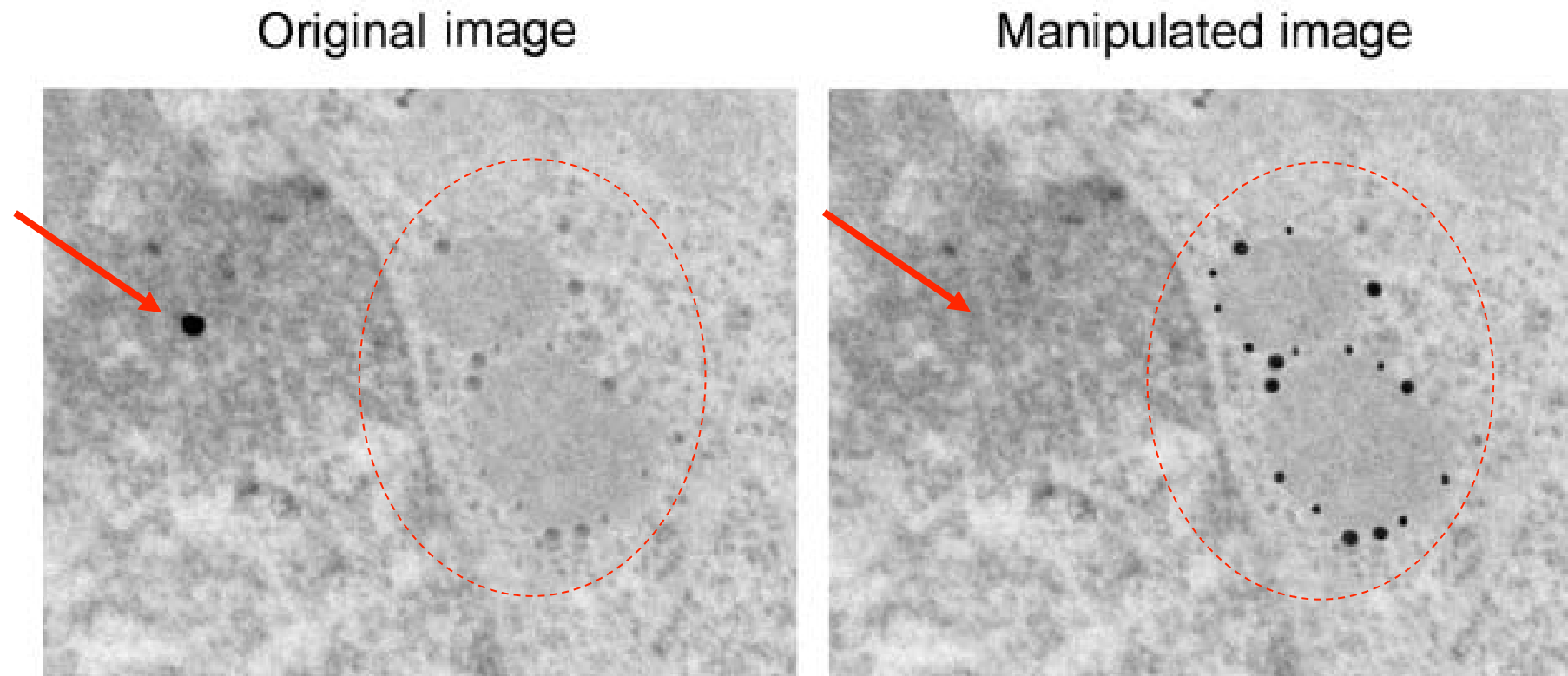
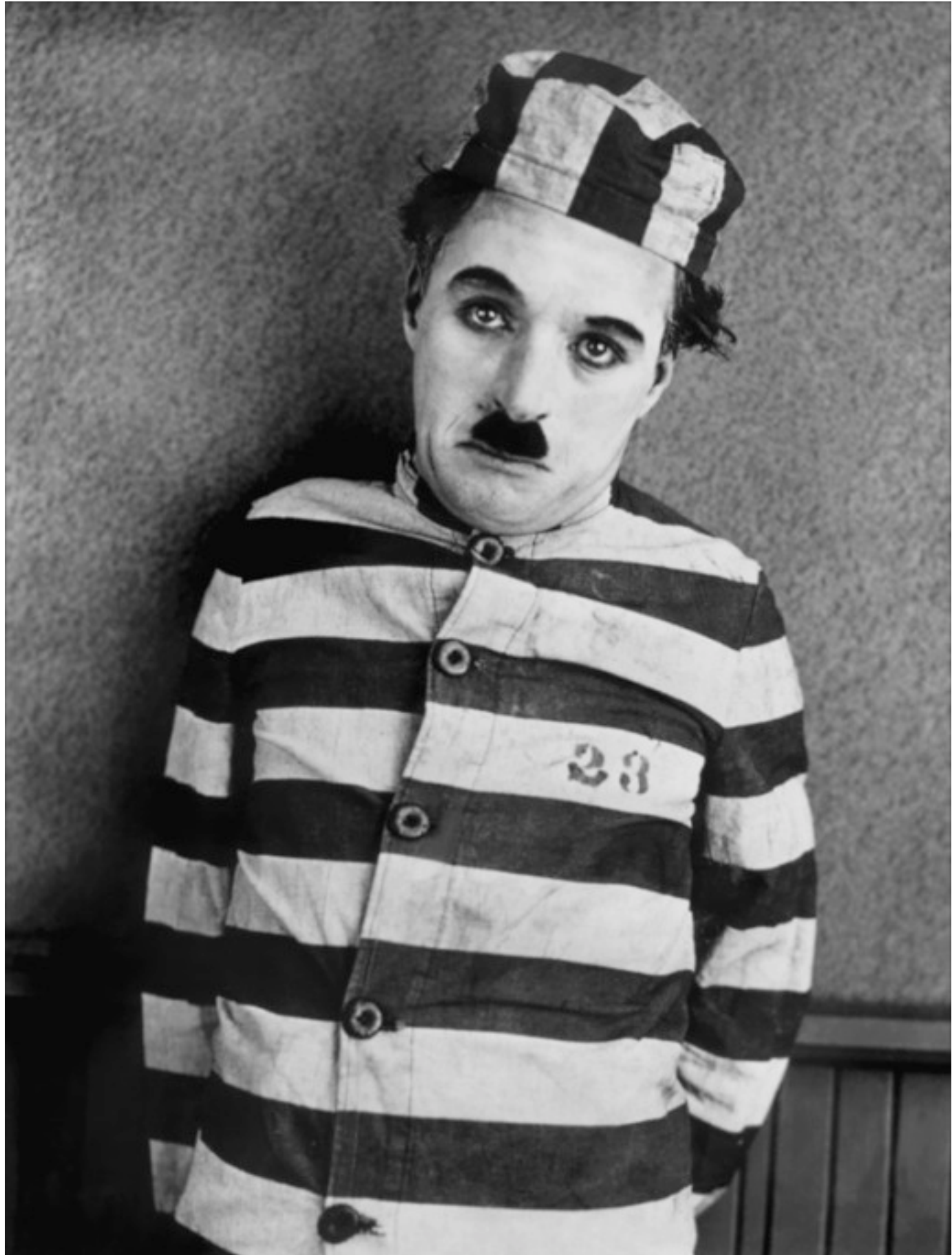


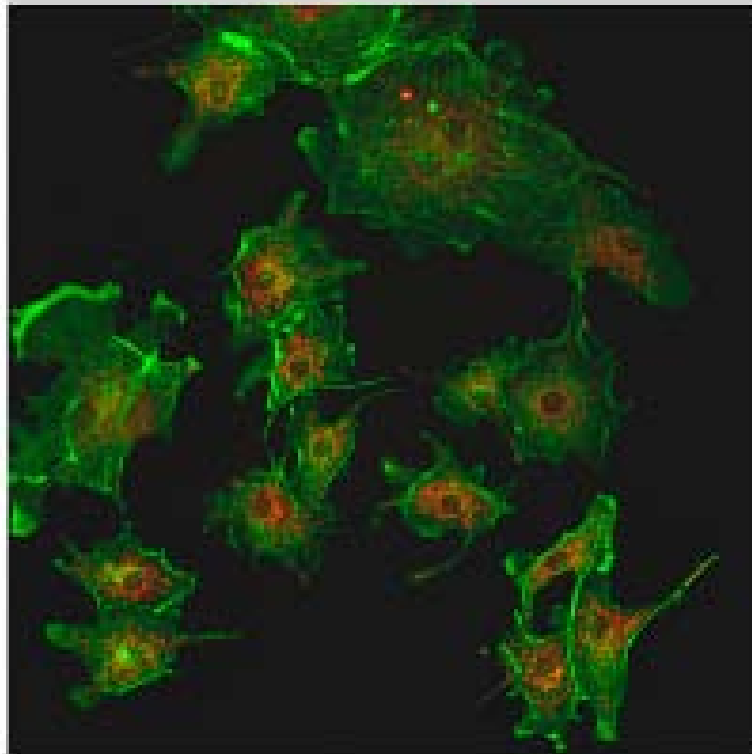
Figure 5. **Misrepresentation of immunogold data.** The gold particles, which were actually present in the original (left), have been enhanced in the manipulated image (right). Note also that the background dot in the original data has been removed in the manipulated image.

- **BAD:** manipulated but **does not alter interpretation**
- **VERY BAD:** Changes interpretation with **intention to defraud**
- **Adjustments necessary to reveal a feature ALREADY PRESENT in the original data are acceptable if they can be justified**

**THEY
HAVE
WAYS
OF
FINDING
OUT
WHAT
YOU
DID!**

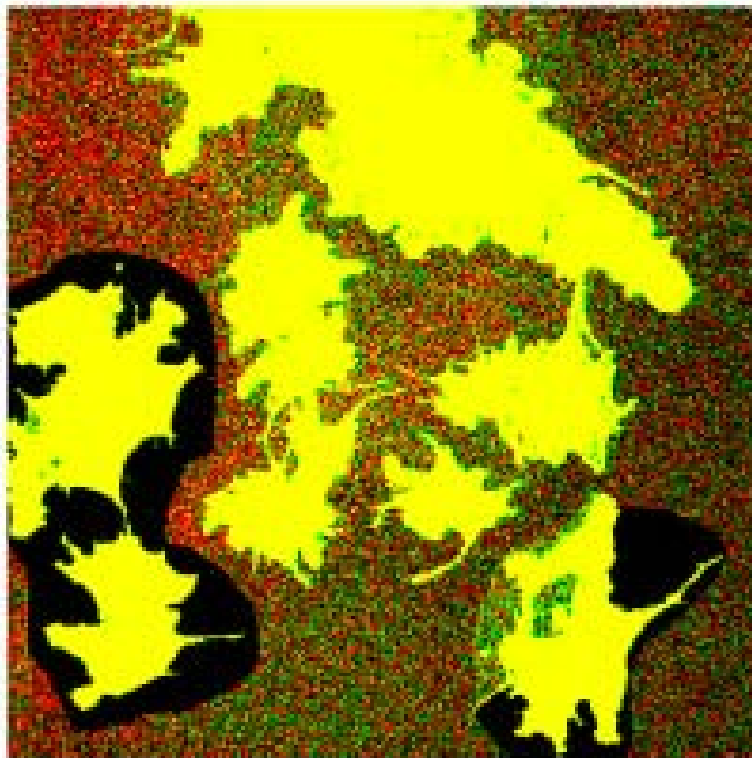


Manipulated
image

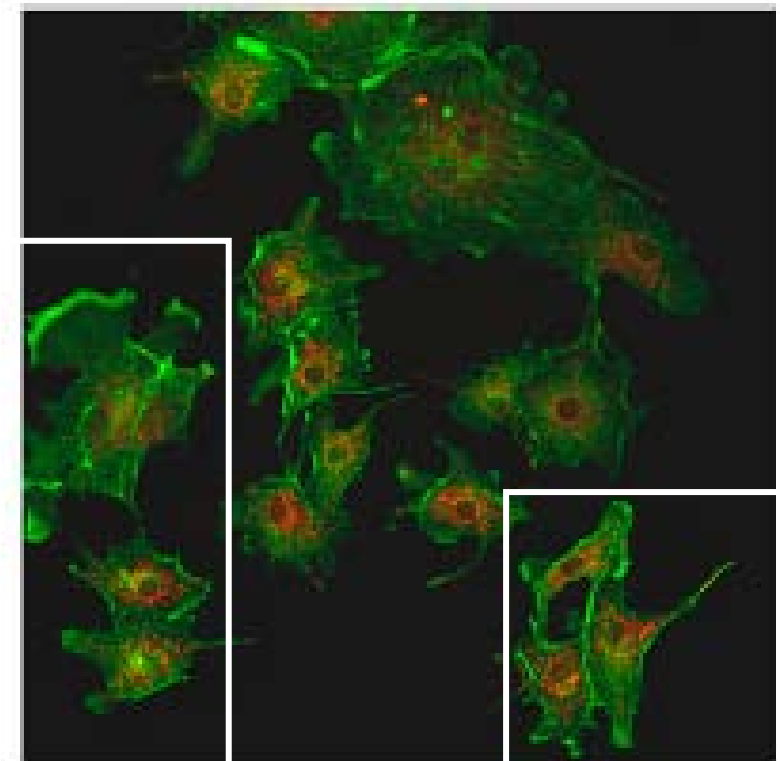


- Miss-representation of cell population within an observed field
- **VERY BAD:** Changes interpretation with **intention to defraud**

Manipulation
revealed
by contrast
adjustment



Correct:



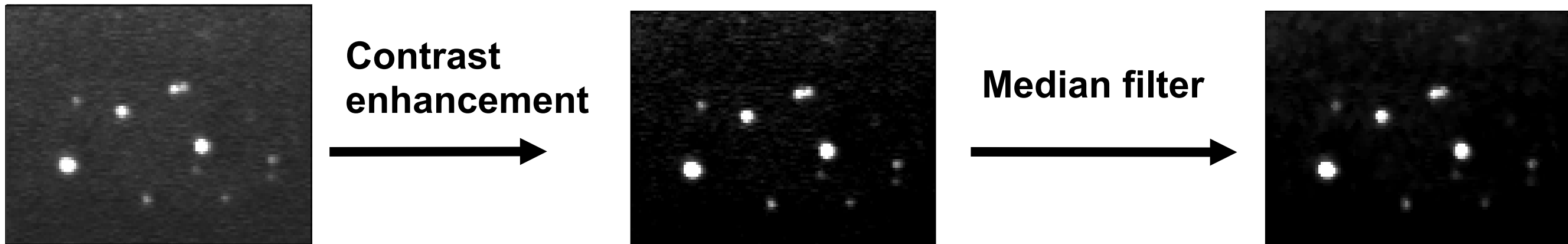
Rossner & Yamada (2004). What's in a picture? The temptation of image manipulation. J. Cell Biology 166: 11–15.

Conceptual Hierarchy of image processing

- **Low - level processing** = Image enhancement (most common)
- **Mid - level processing** = Features and attributes extracted
- **High - level processing** = Interpretation of images

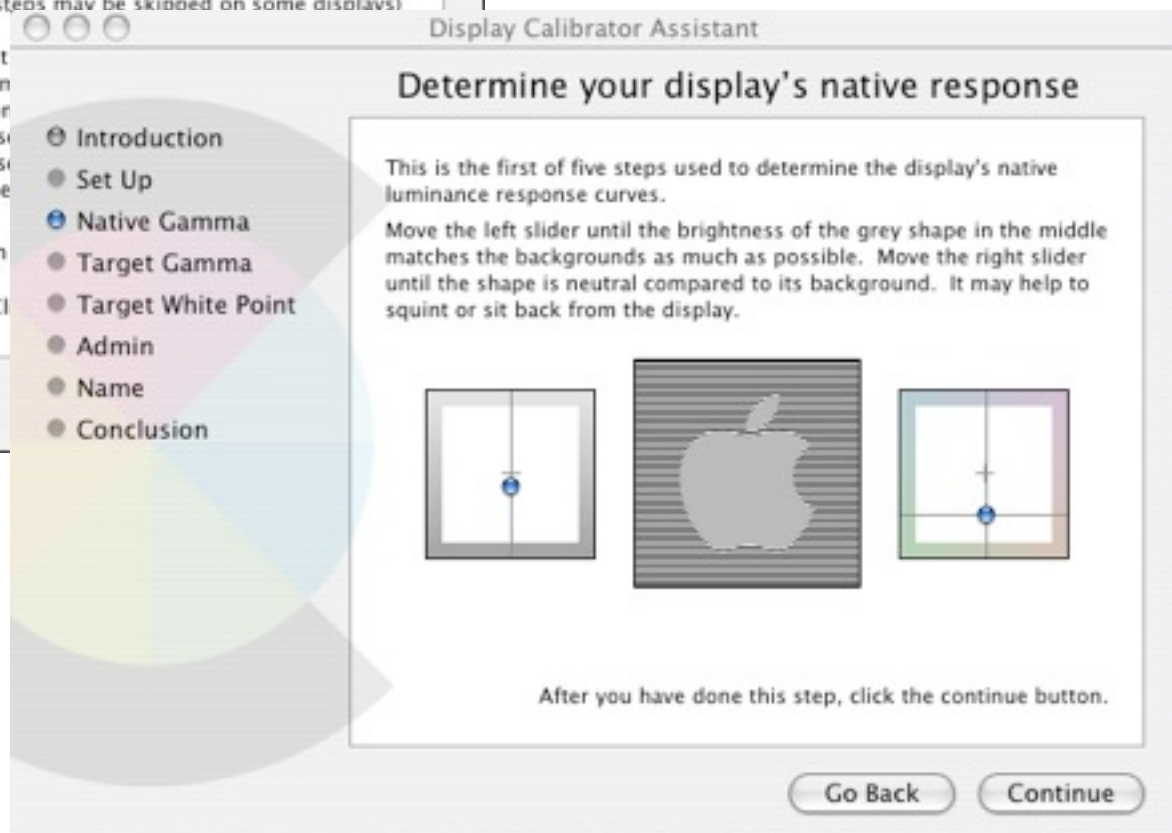
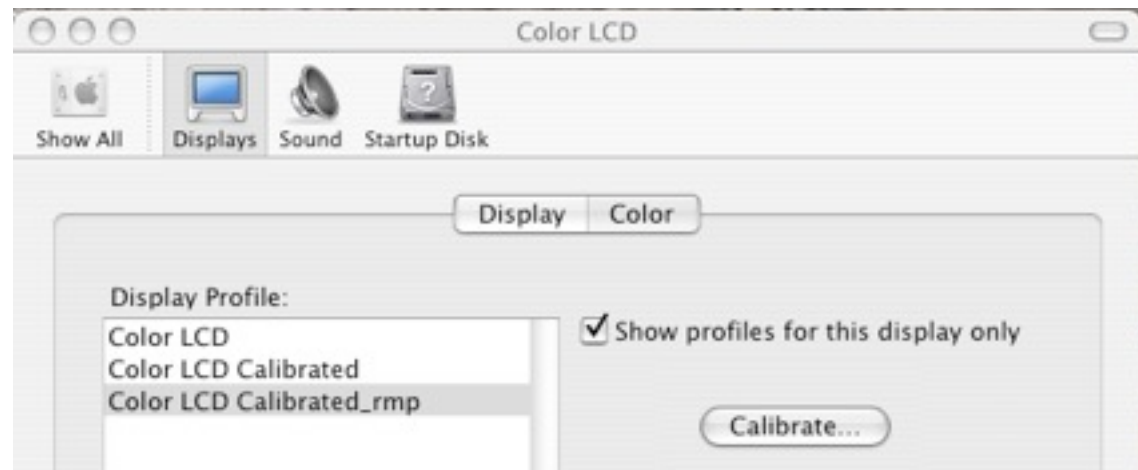
LOW LEVEL Processing

- Visual enhancement
 - Subjective = looks better
 - Input is an **image**, output is an **image**
-
- Adjustments for image **Display** / Printing
 - Enhancement **Filters**
 - Deconvolution



LOW LEVEL Processing - Display, monitor setup

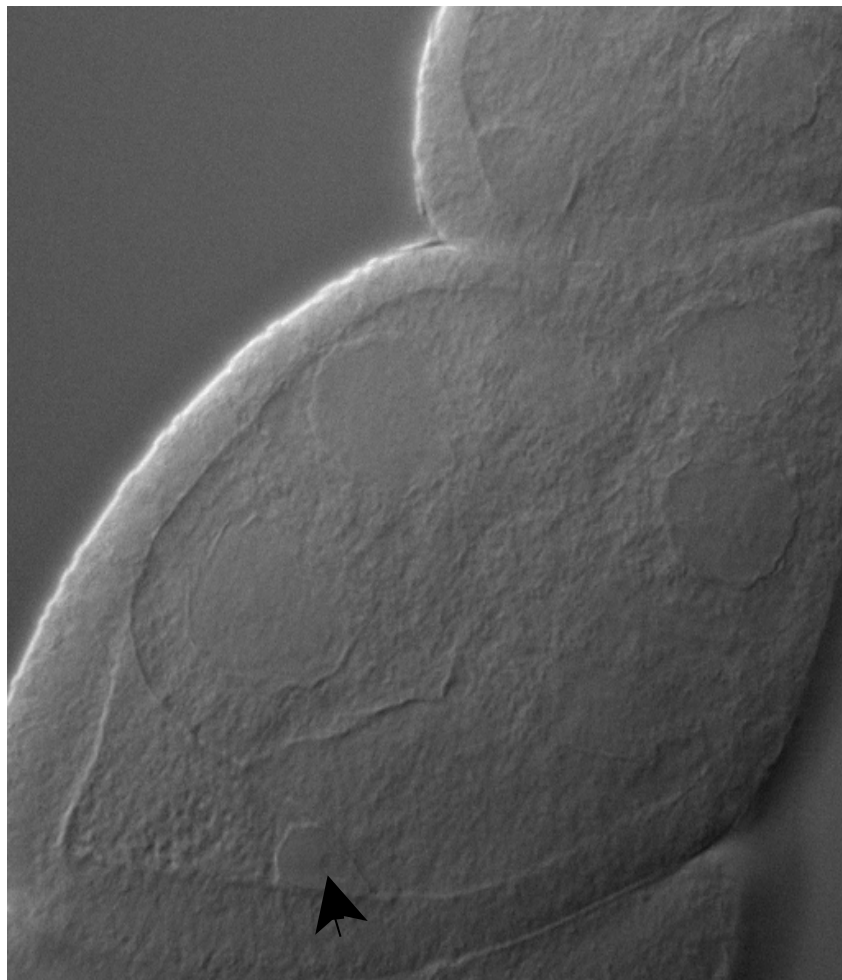
Monitor calibration tools - Mac OSX (system preferences, Displays, Colour)



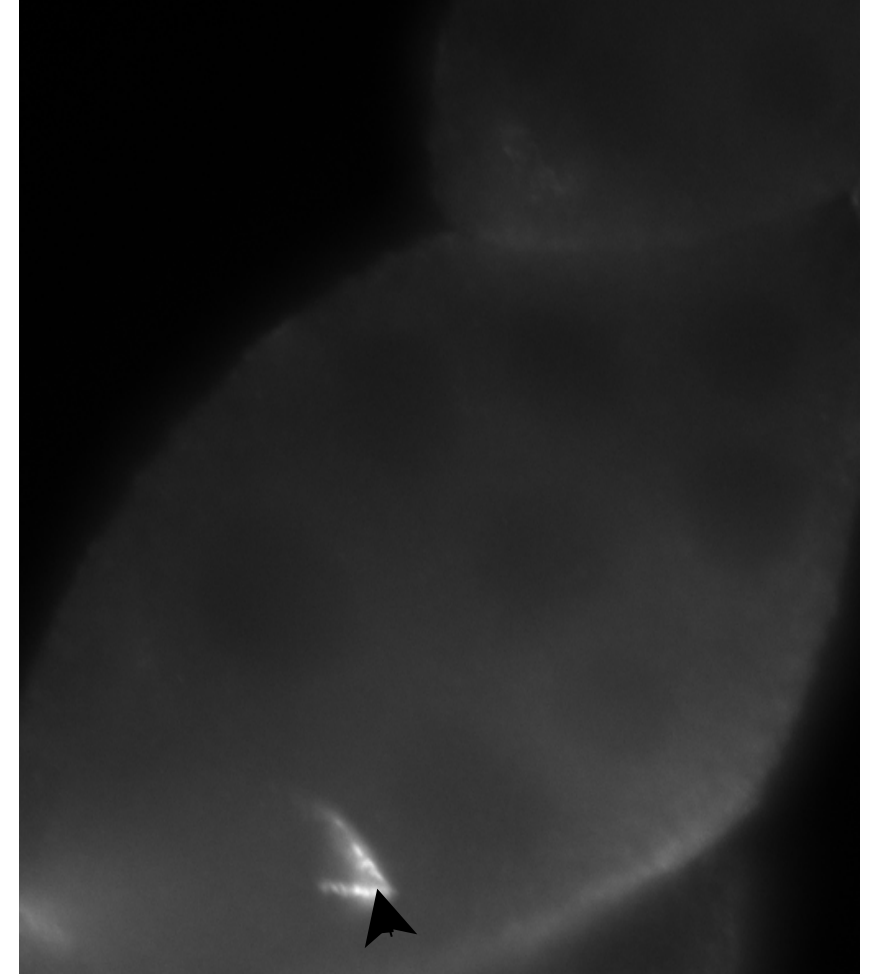
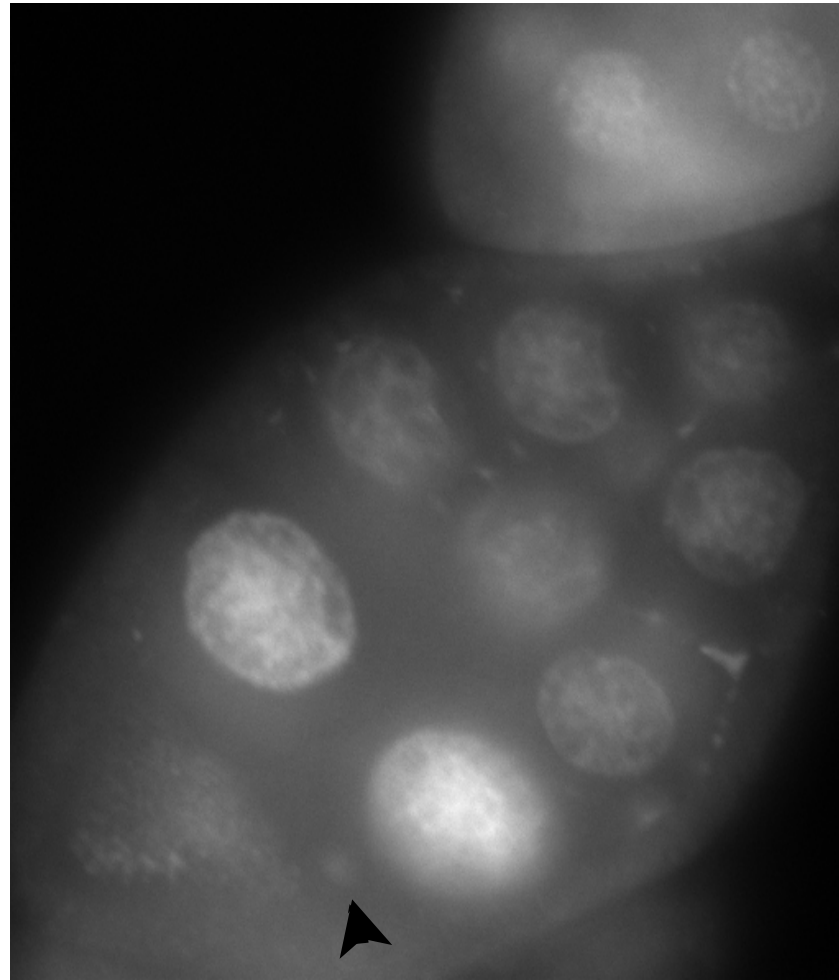
<http://epaperpress.com/monitorcal/>
<http://www.bodoni.co.uk/profiling/colourprofiling.html#monitor>
<http://www.bodoni.co.uk/profiling/spyder.html>

LOW LEVEL Processing - Display, Grey Scale

DIC/DAPI/Grk in situ - grey scale images



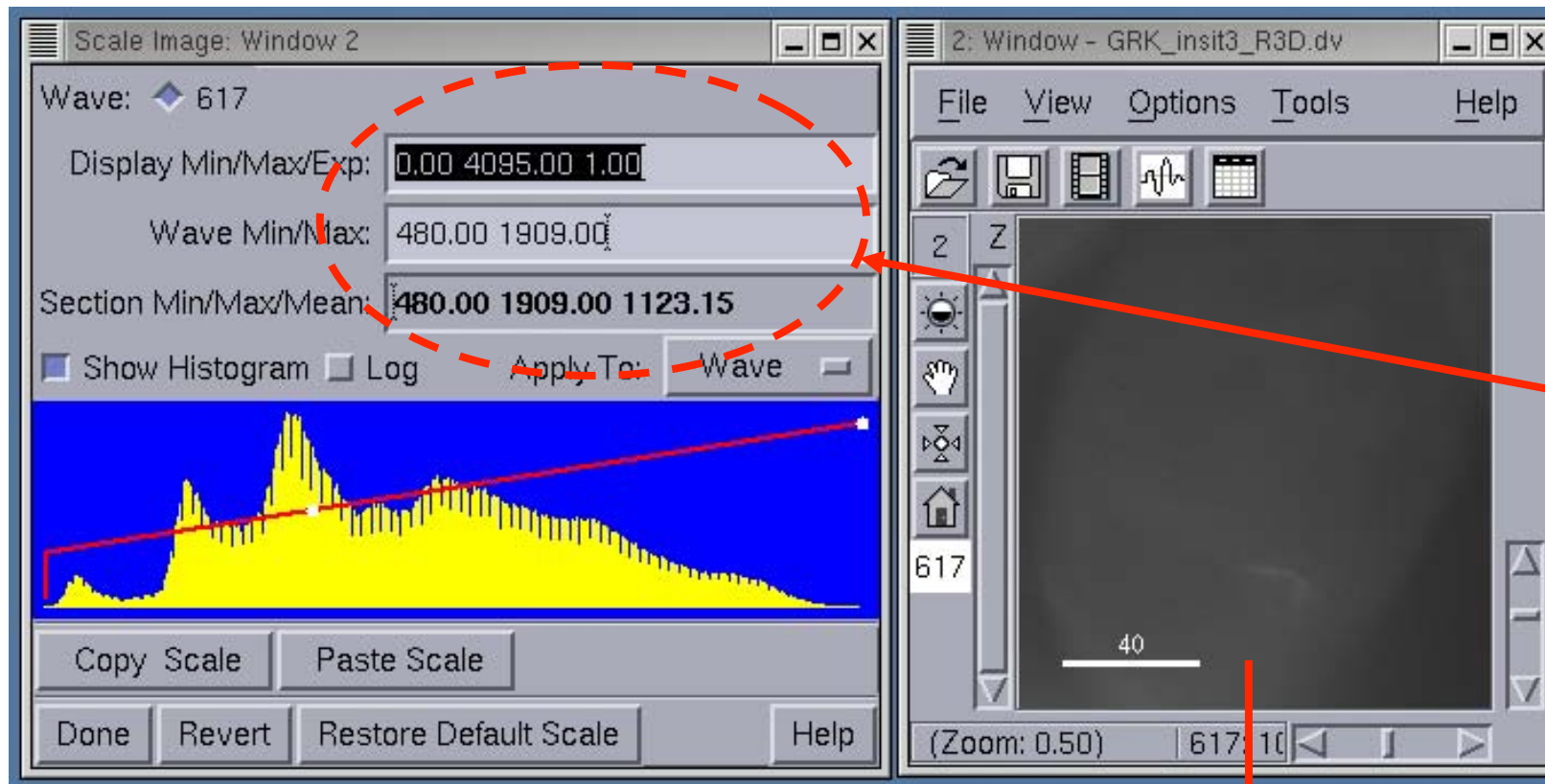
(arrowhead marks the oocyte nucleus)



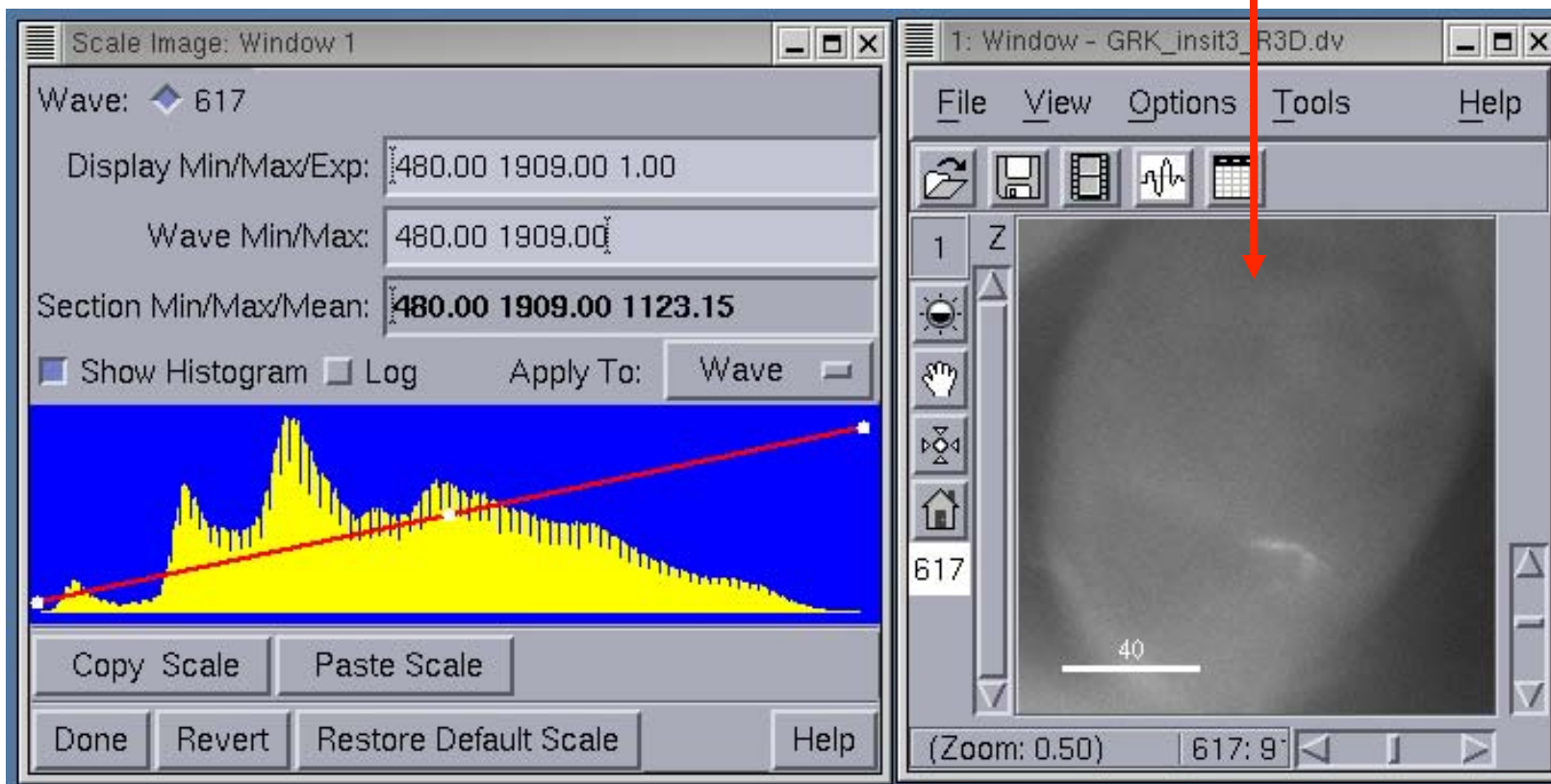
- For viewing and display use **grey scale** scale images to see fine detail.

LOW LEVEL Processing - Display, Brightness/Contrast

- **Brightness and contrast** - Enhancing details which are too close in grey level to be easily discernible.



Better to set your contrast by **numbers** to make the operation more systematic
0-4095 is full range for 12 bit



Auto-intensity scaling by softWoRx scales **the display** to fill the dynamic range

Display Brightness and contrast

Image series collected by decreasing the excitation lamp intensity from 100% to 50%, 10%, 1%, and 0.1%

Scaled 0 - 4095

Full Dynamic range

50% Dynamic range

10% Dynamic range

1% Dynamic range

0.1% Dynamic range

Auto Intensity Scaled display

Decreasing signal

Increasingly
Noisy looking

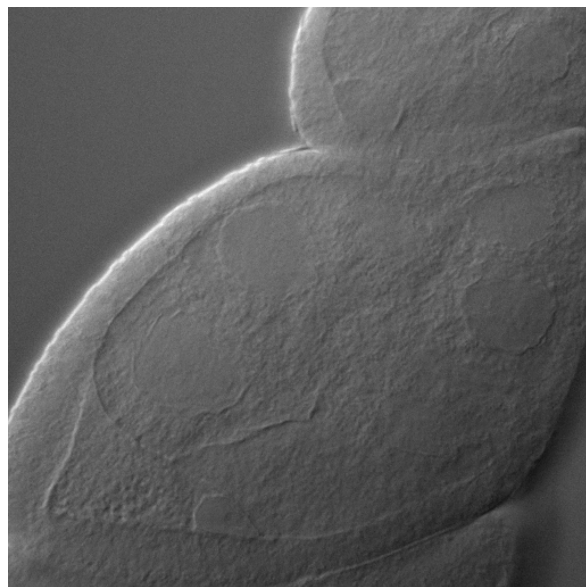
Decreasing
Image quality

Cannot resolve

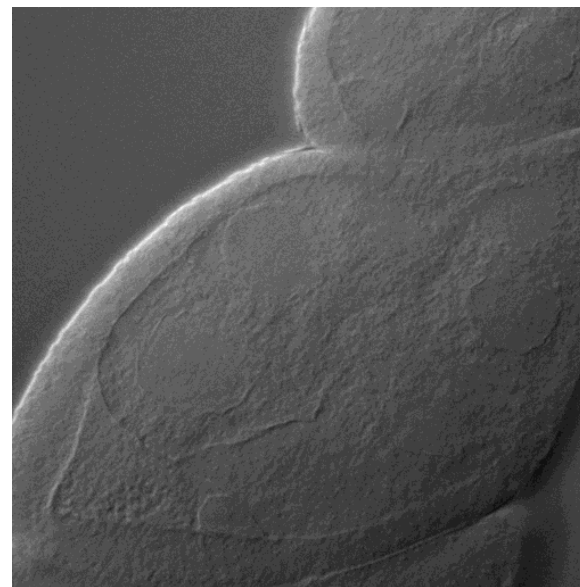
LOW LEVEL Processing - Display, Bit Depth (levels)

- Eye has limited ability to distinguish grey levels/colours
Above 32 grey levels images look smooth - 16 and below grey levels eye perceives objectionable banding = **false contours**.

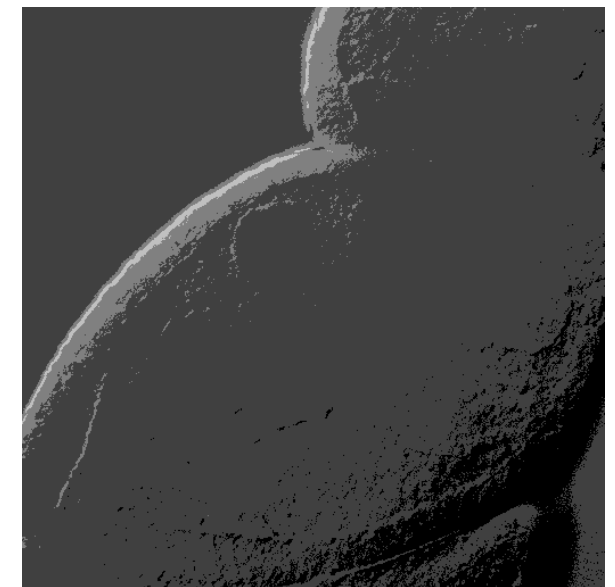
False contouring due to insufficient grey levels



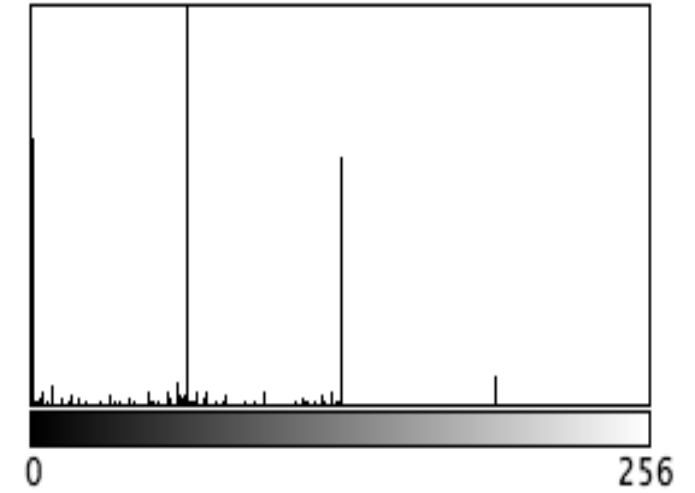
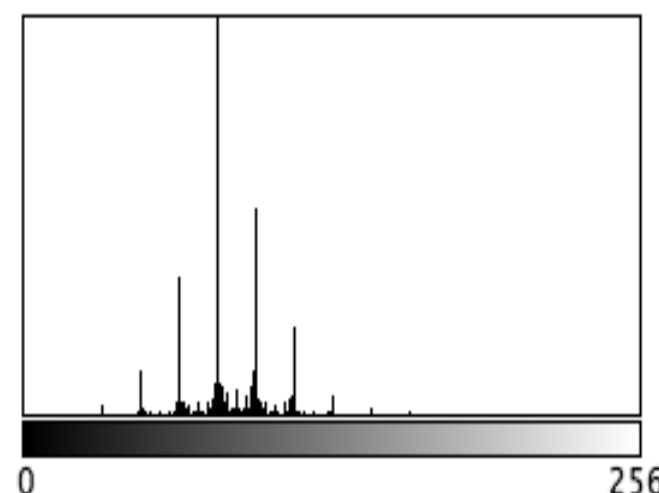
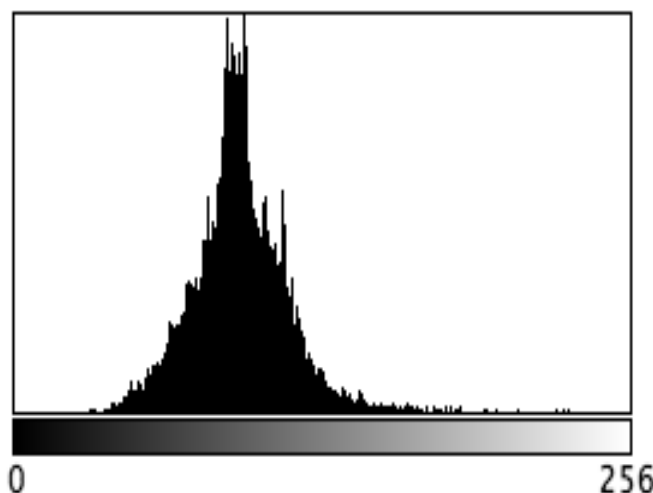
256 greys



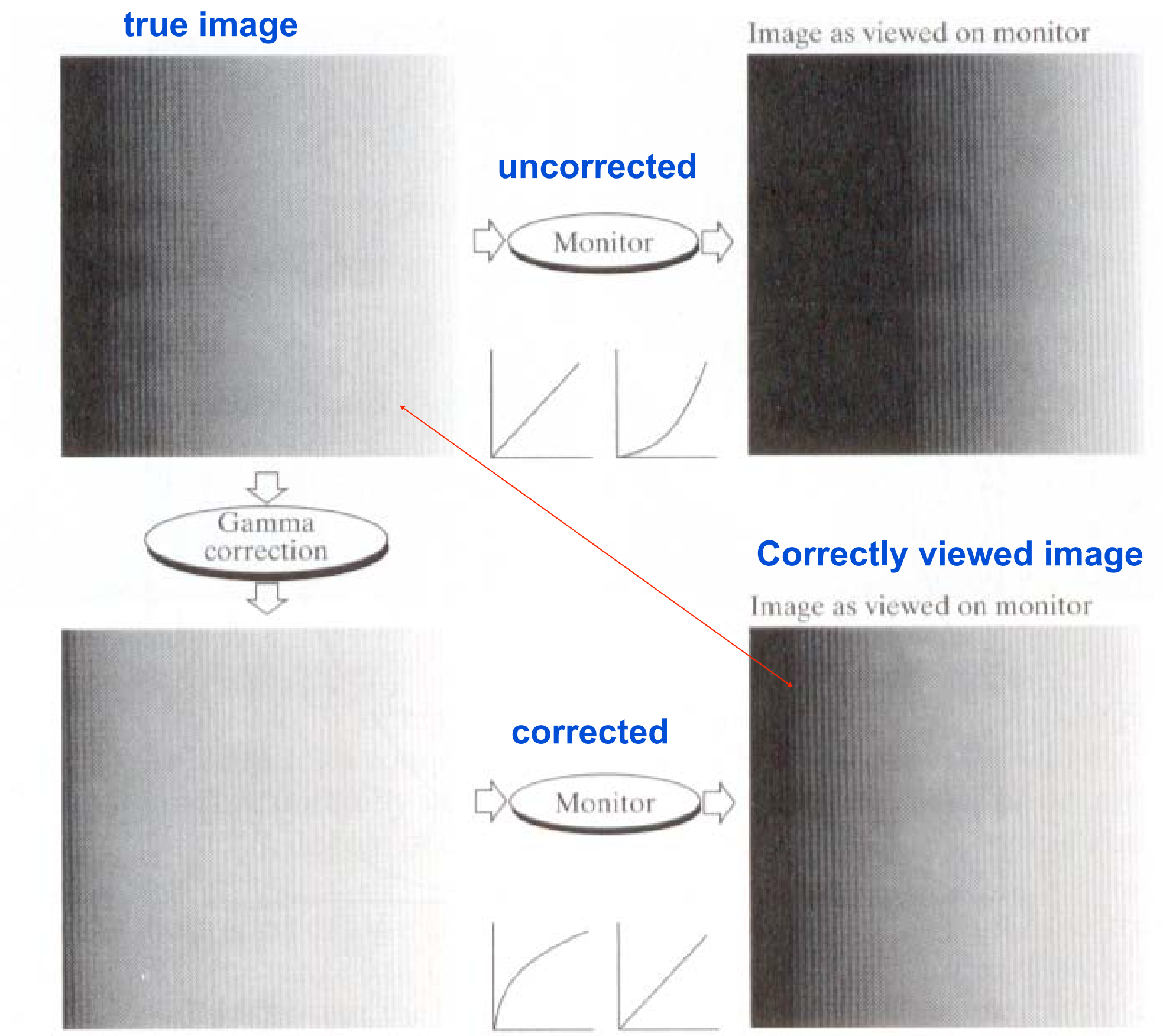
16 greys



4 greys

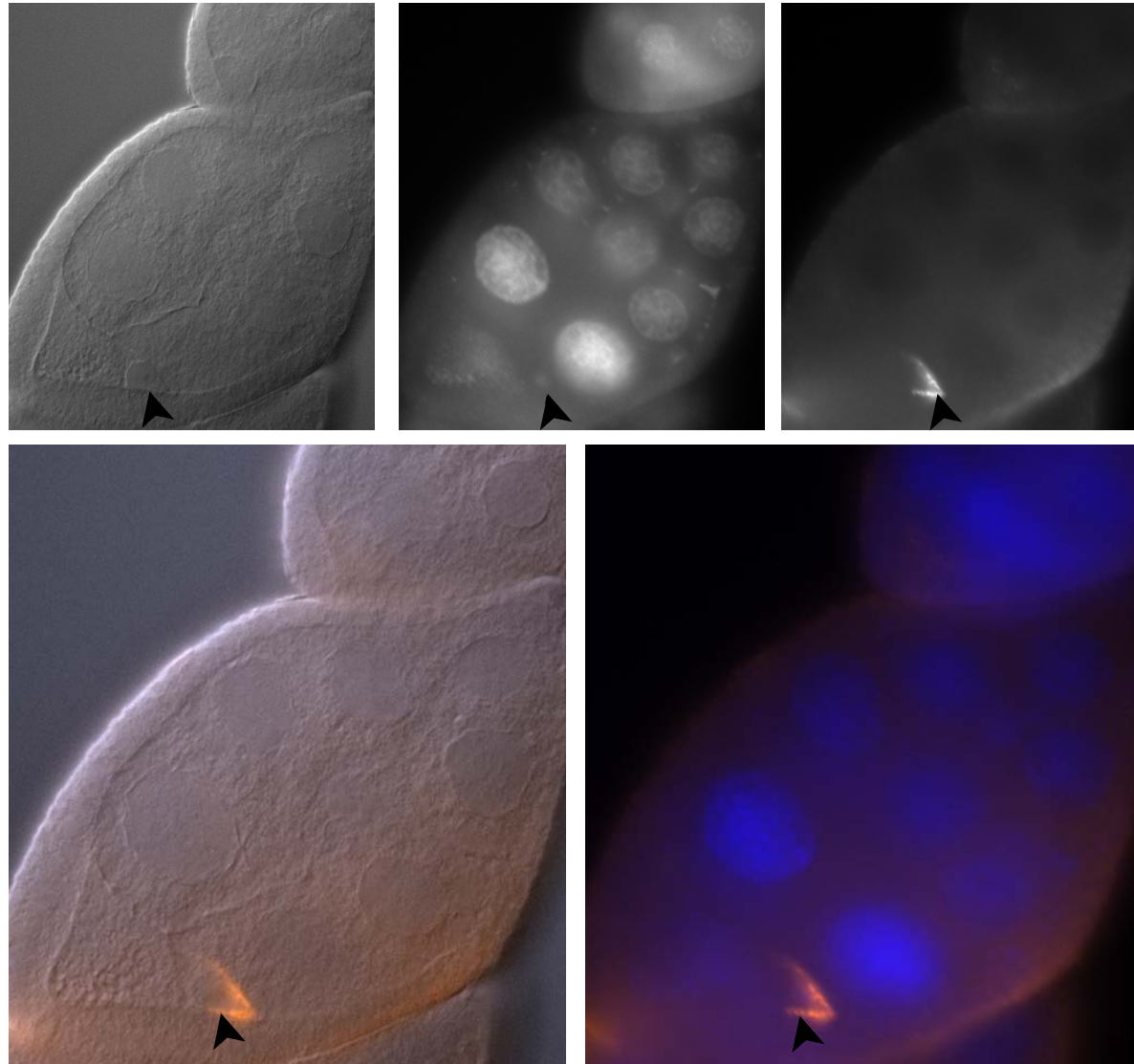


LOW LEVEL Processing - Display, Using Gamma



LOW LEVEL Processing - Display, Colour

DIC/DAPI/Grk in situ - grey scale images, colour blended, additive overlays

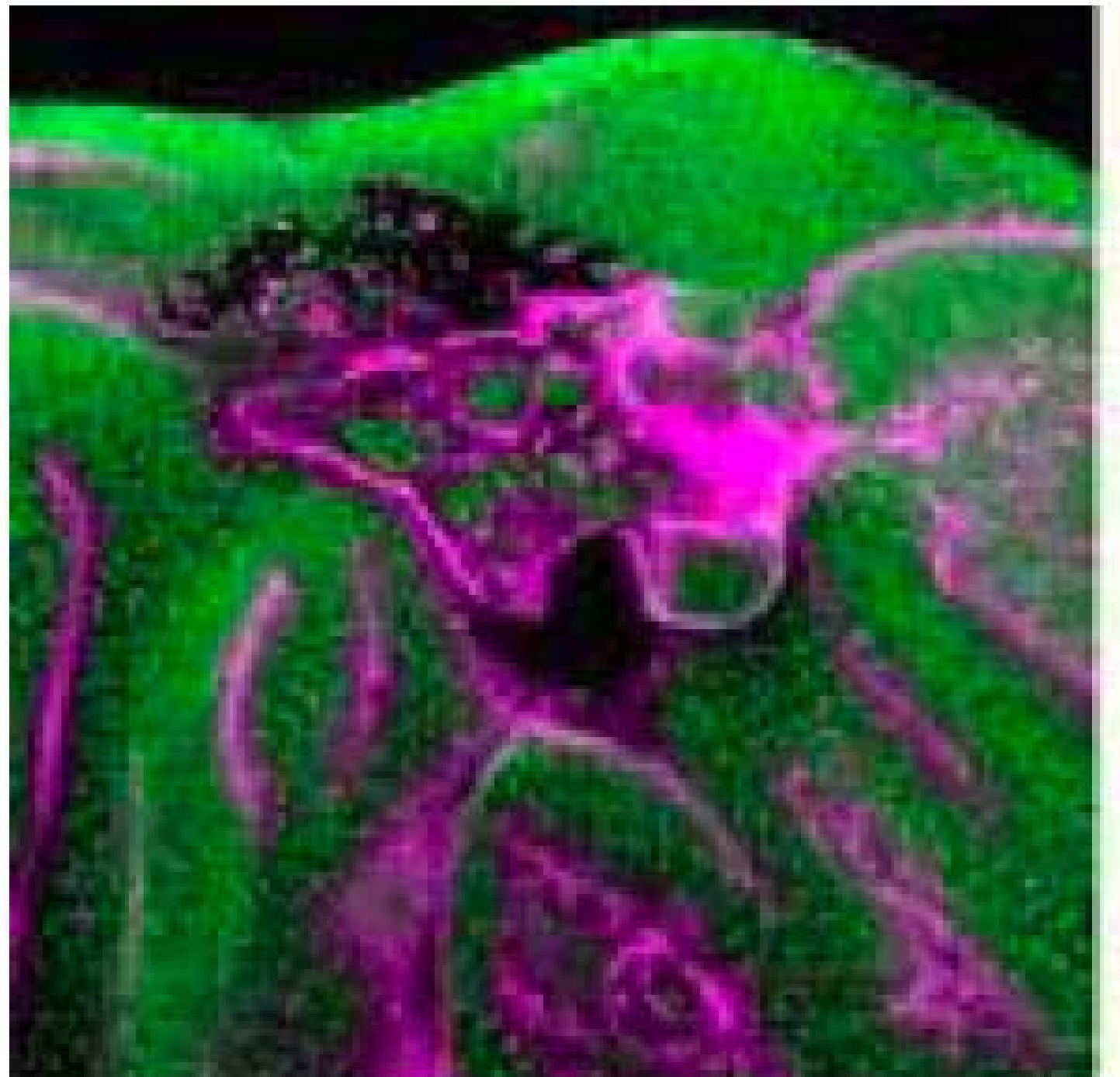
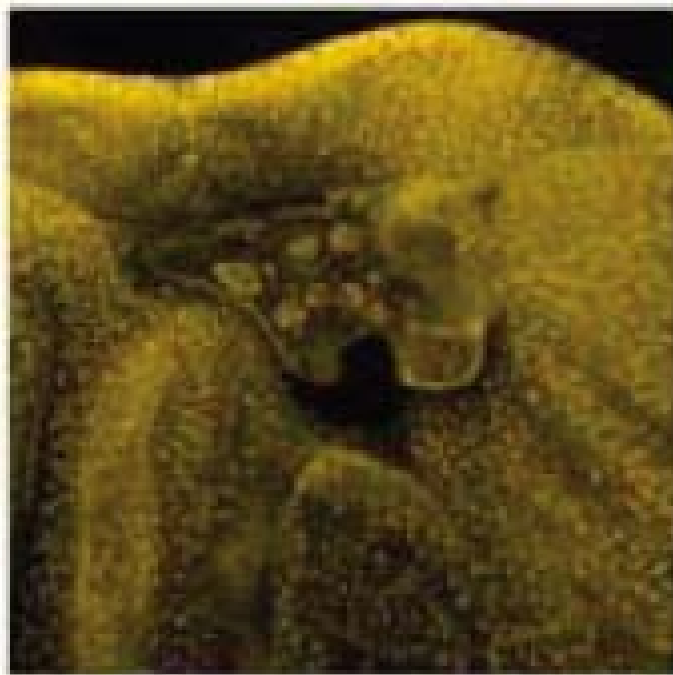
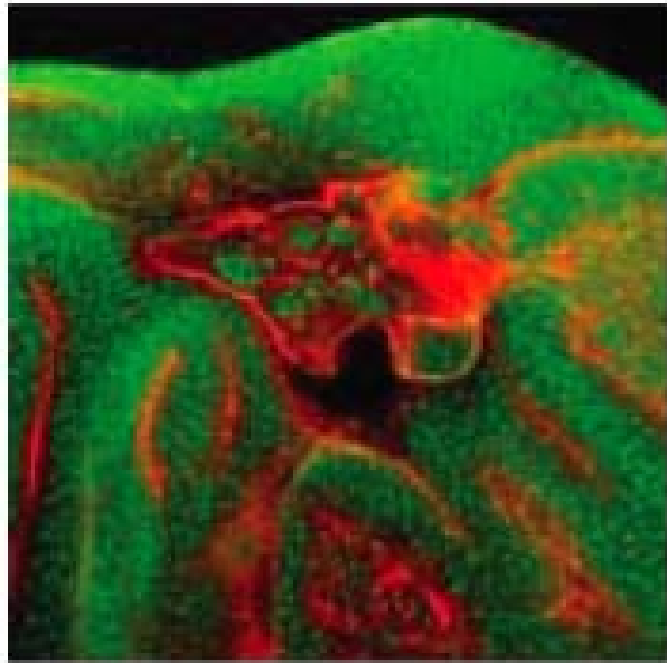


(arrowhead marks the oocyte nucleus)

- Colour should be used for **highlighting particular intensity differences / co-localisation**.
- For publication show greyscale images alongside colour overlays.
- Consider colour-blind friendly colours: green / magenta / white.

LOW LEVEL Processing - Display, Colour

- Consider colour blind friendly colours: magenta, green



LOW LEVEL Processing - Display, Making Movies

- Movie formats: .avi; .mov; (.mpeg)

- Considerations:

 - image **quality vs movie size** (use of compression).

 - speed of play** (frames / second).

 - speed of play on the computer may be slowed by large movies

- ImageJ

 - Will open many file formats and **export straight to .avi or .mov.**, also can open tif image series (image001.tif; image002.tif; etc) restack and export to .avi or .mov. Has **compression options** for .mov

- Quicktime Pro 7

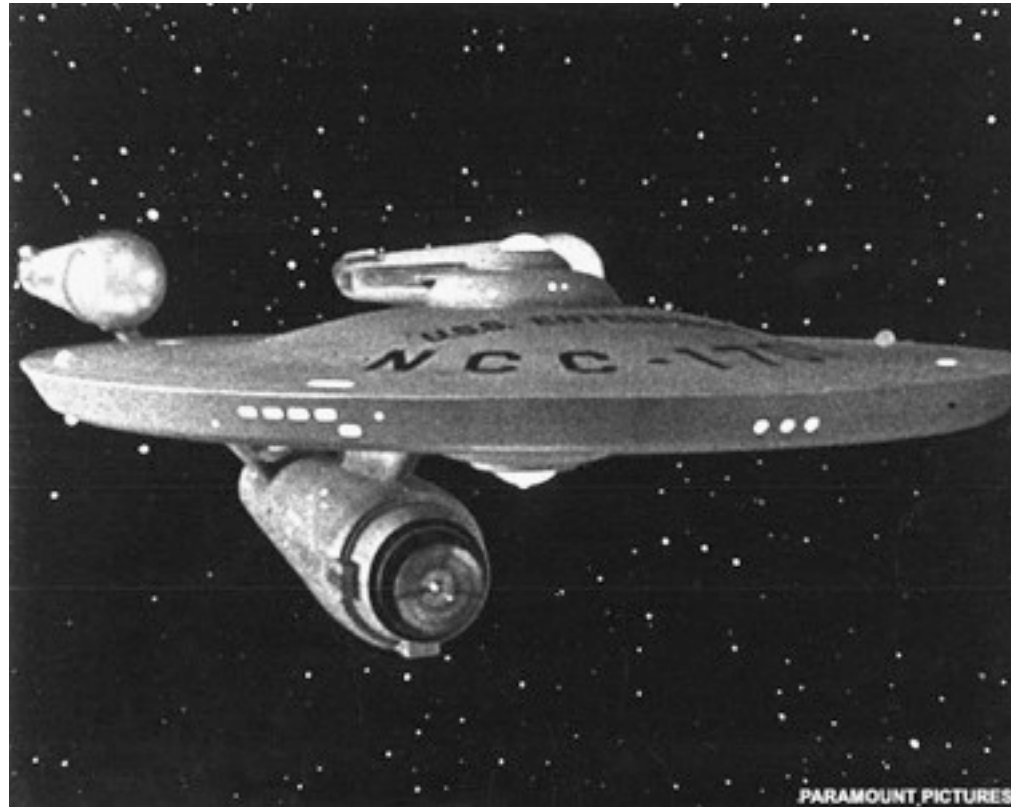
 - Can **open tif image series and export to .avi or .mov**

 - Can **interconvert movie formats.**

 - Has a range of **compression options** for .mov

LOW LEVEL Processing - Simple filtering

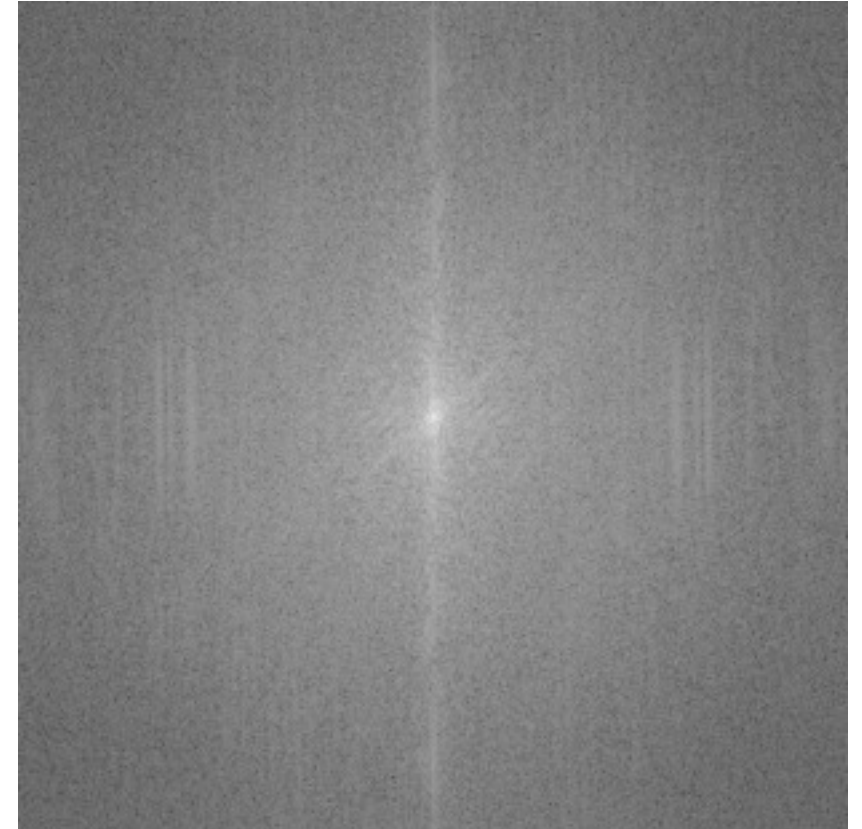
Processing in
Real Space



or

Frequency Space

Fourier
Transform
→



Example:

- **Noise reduction filtering** using a spatial filtering mask – **3x3 median filter**
- **Noise reduction filtering** in the frequency domain – **Fourier bandpass filter**

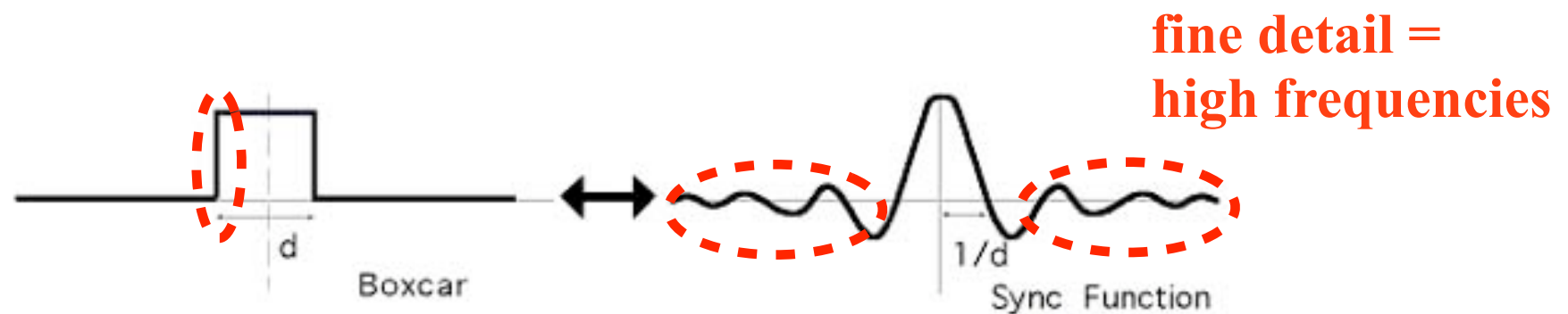
Fourier Space = Frequency space
= Reciprocal space
= K space

Data is broken down into its “frequency” components

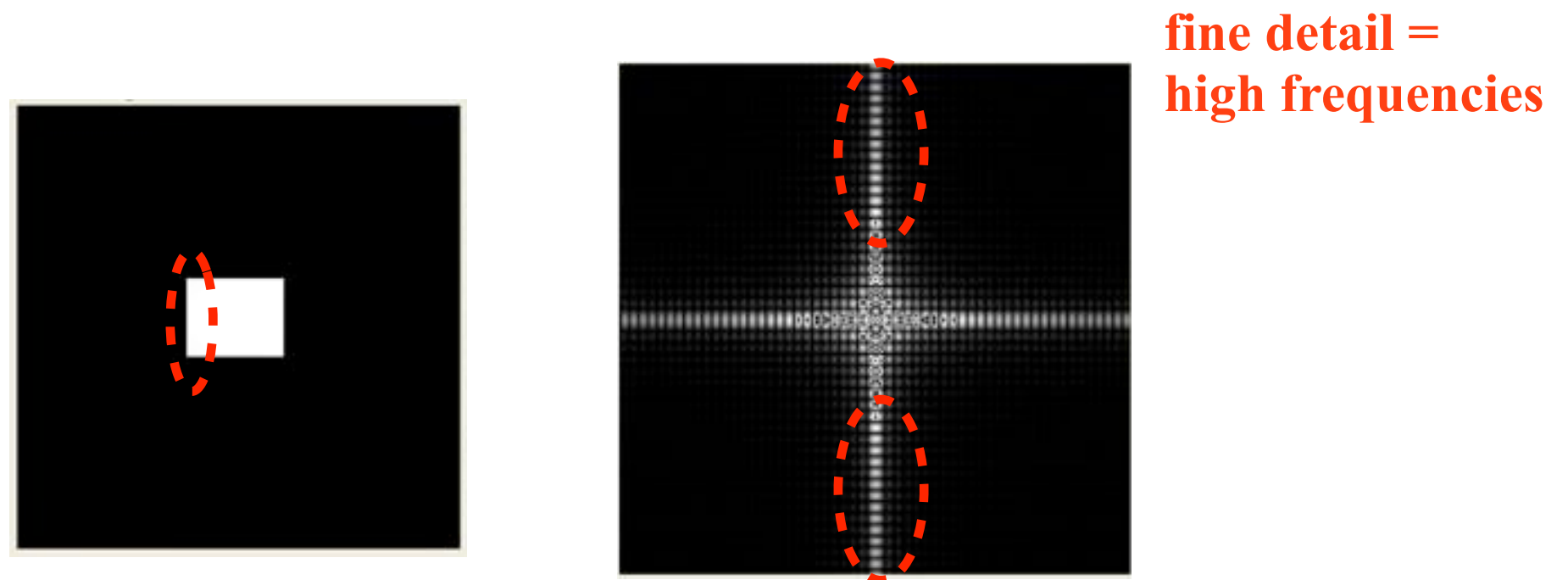
real space

reciprocal space

1D case



2D case



LOW LEVEL Processing - Simple filter, spatial domain

- Real space - pixel by pixel

e.g. Noise reduction filtering using a 3x3 median filter

MEDIAN 3x3:

Replaces value of a pixel by the median grey scale value of the ranked values of the 9 neighbourhood pixels.

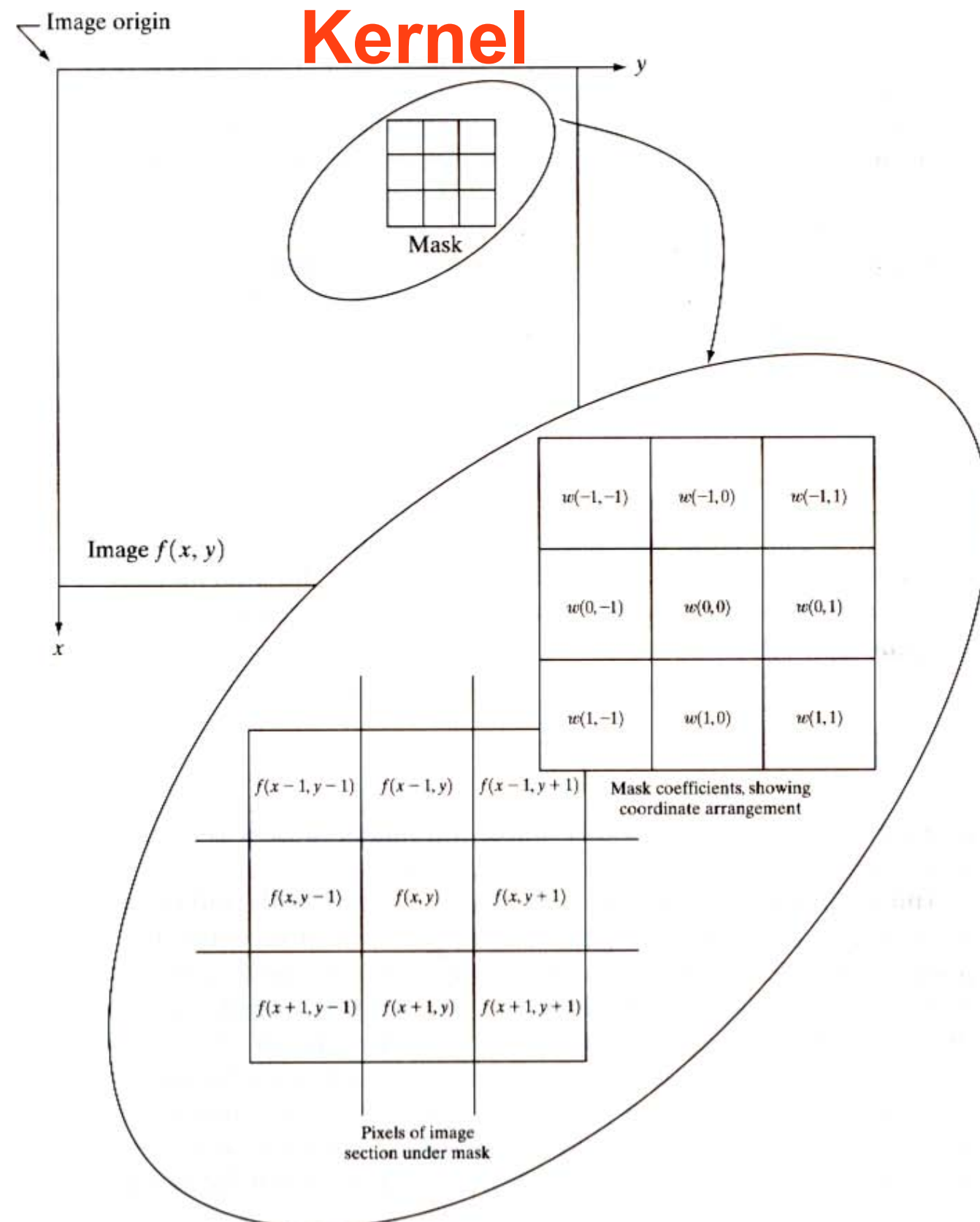
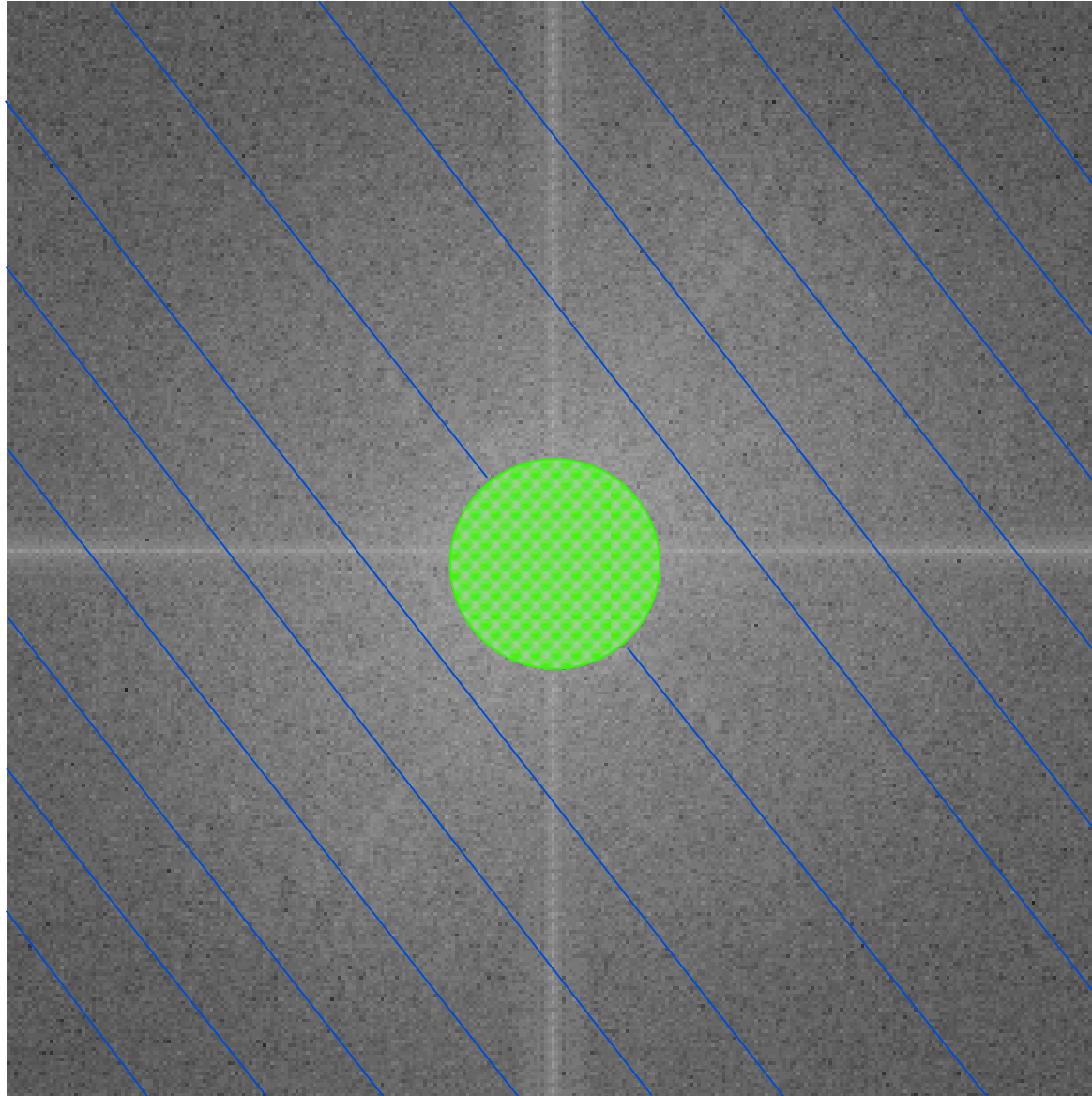


FIGURE 3.32 The mechanics of spatial filtering. The magnified drawing shows a 3×3 mask and the image section directly under it; the image section is shown displaced out from under the mask for ease of readability.

LOW LEVEL Processing - Simple filter, Fourier domain

- **Frequency space** - **all the image at once, computationally easier**
- Requires you to “transform” your image into **Reciprocal** or **Fourier** space
e.g. in ImageJ: process, FFT (fast Fourier transform)



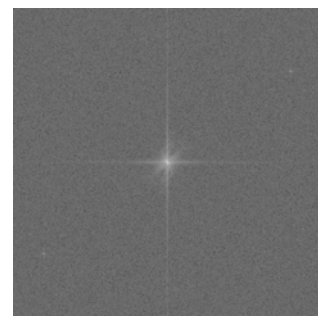
Low frequencies = **coarse detail**

High frequencies = **fine detail and noise**

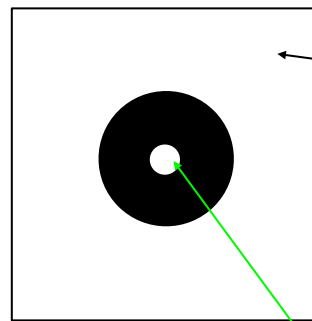
LOW LEVEL Processing - Simple filter, Fourier domain

- **Frequency domain** - images converted to **Fourier space**

e.g. Noise reduction using a low pass or band pass filter



x



Fourier “mask” selectively eliminates the highest frequencies = noise and very fine detail.

Can also eliminate large expanses of even intensity - low frequencies

Works on the whole image at once

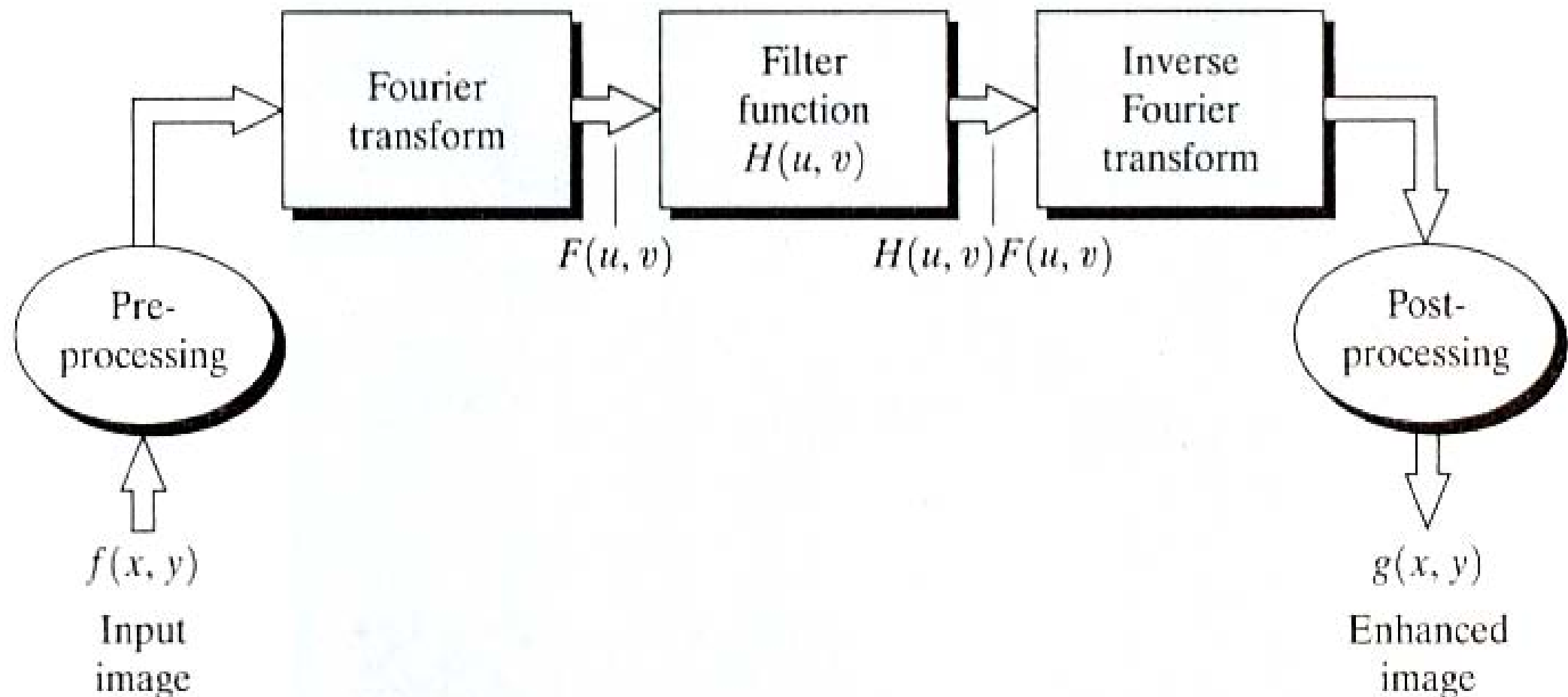
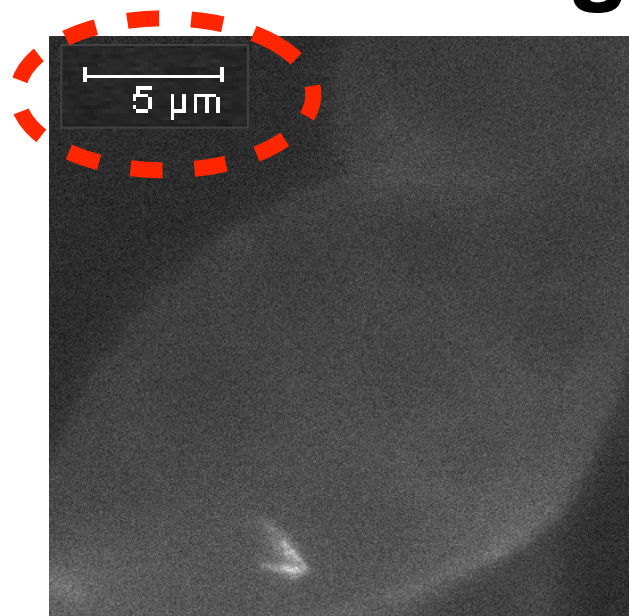


FIGURE 4.5 Basic steps for filtering in the frequency domain.

Noise Filtering

limited use when resolving fine detail!

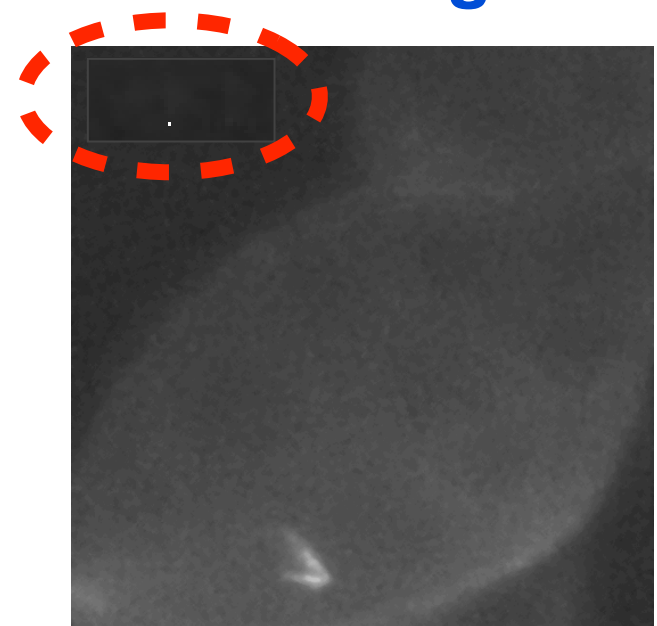


Noisy image

Spatial domain processing

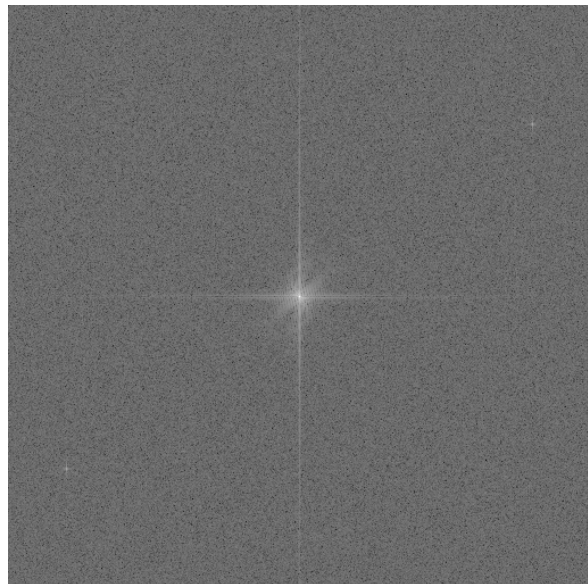


3x3 Median
(high pass filter)



Noise reduced
Some false contours

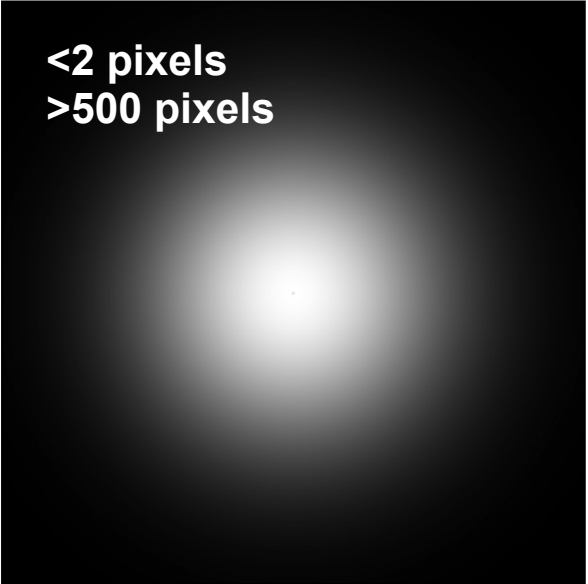
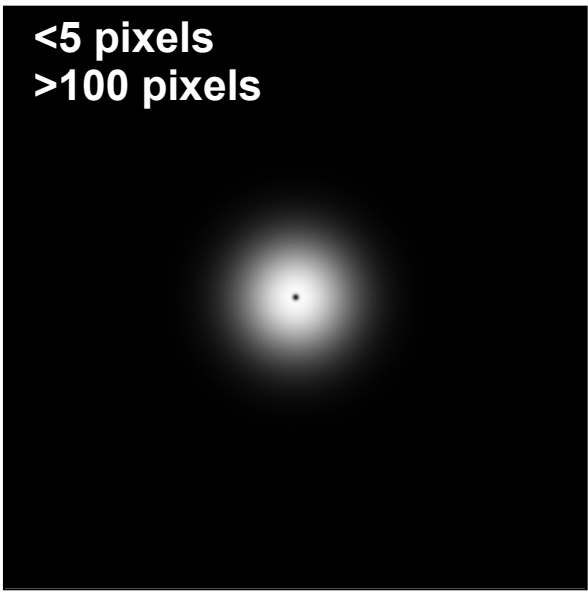
Fourrier
transform



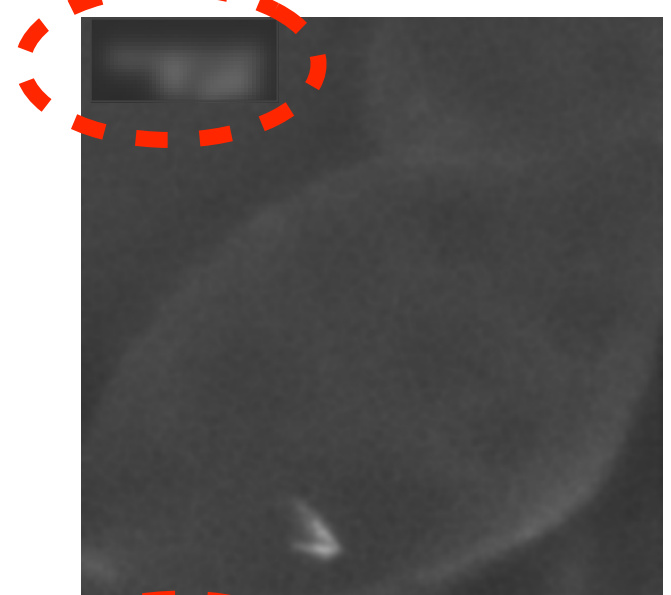
X



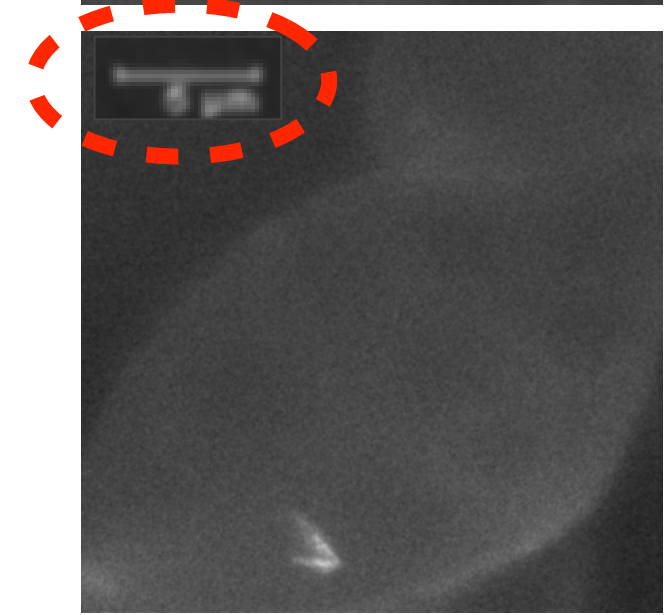
Band pass filters (mask)



Selected frequencies eliminated

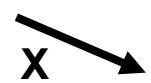


inverse
Fourrier
transform



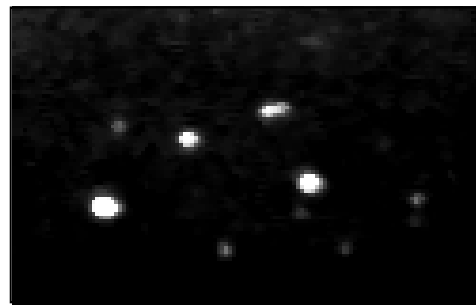
Frequency domain processing

X

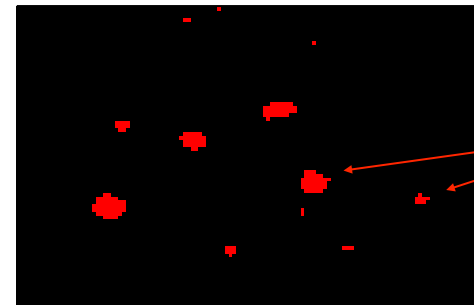


MID LEVEL Processing

- Input is an **image**, output is an **attribute extracted from the image**



Segmentation



**Objects
defined**

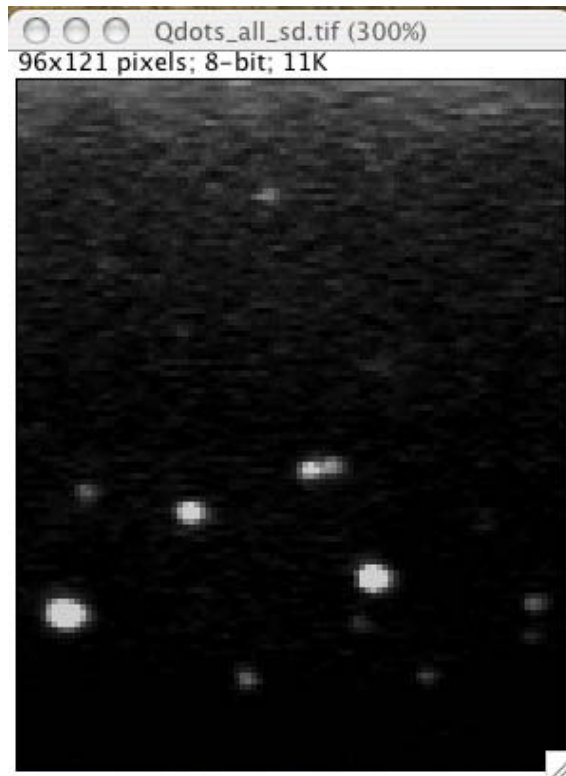
**Number of objects
Positions of objects
Size of objects**

**Also:
- Colocalisation**

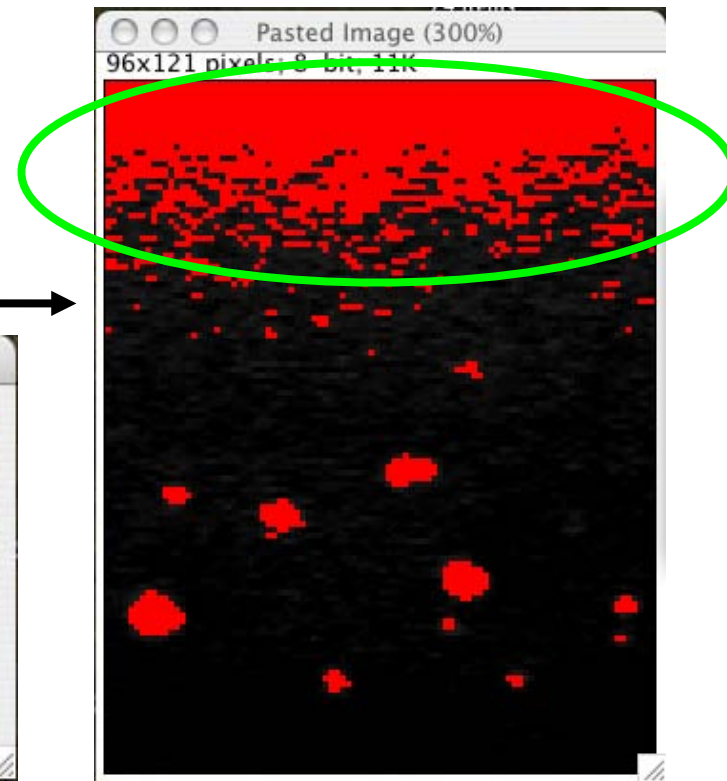
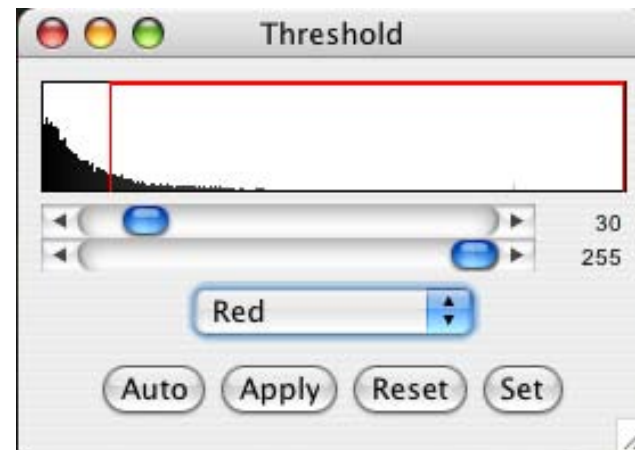
(See appendices)

MID LEVEL Processing - simple segmentation

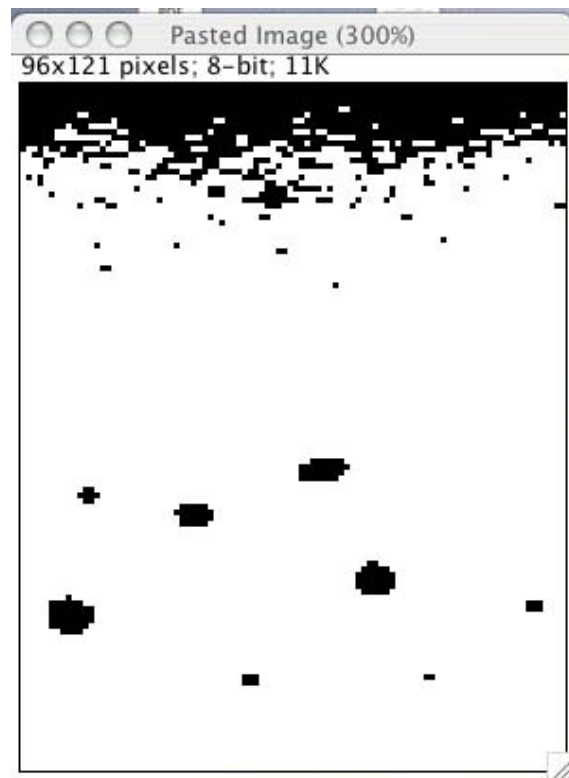
53



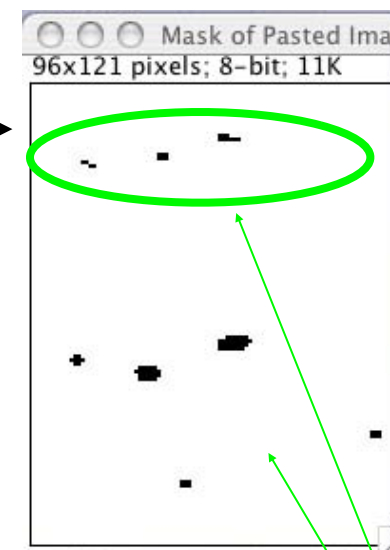
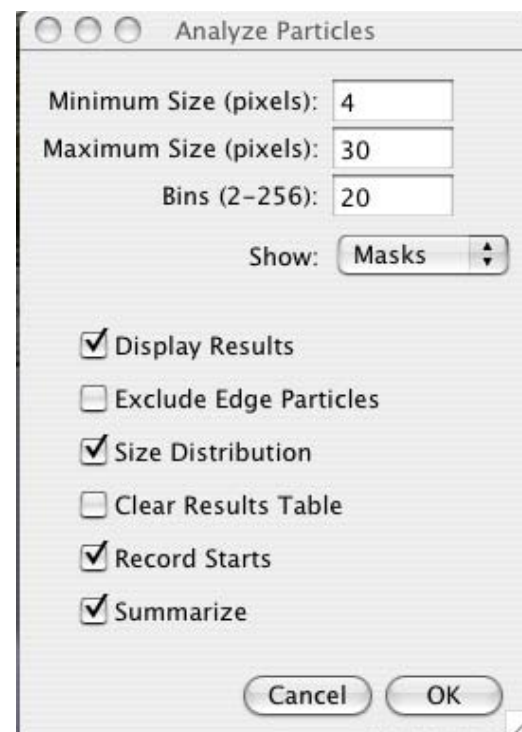
Segment by **intensity**



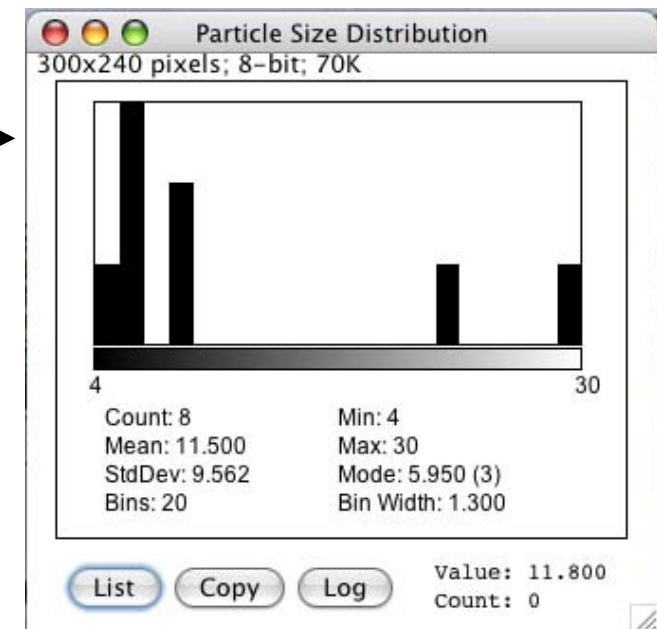
problem region



Segment again by **area size**



mask defining regions

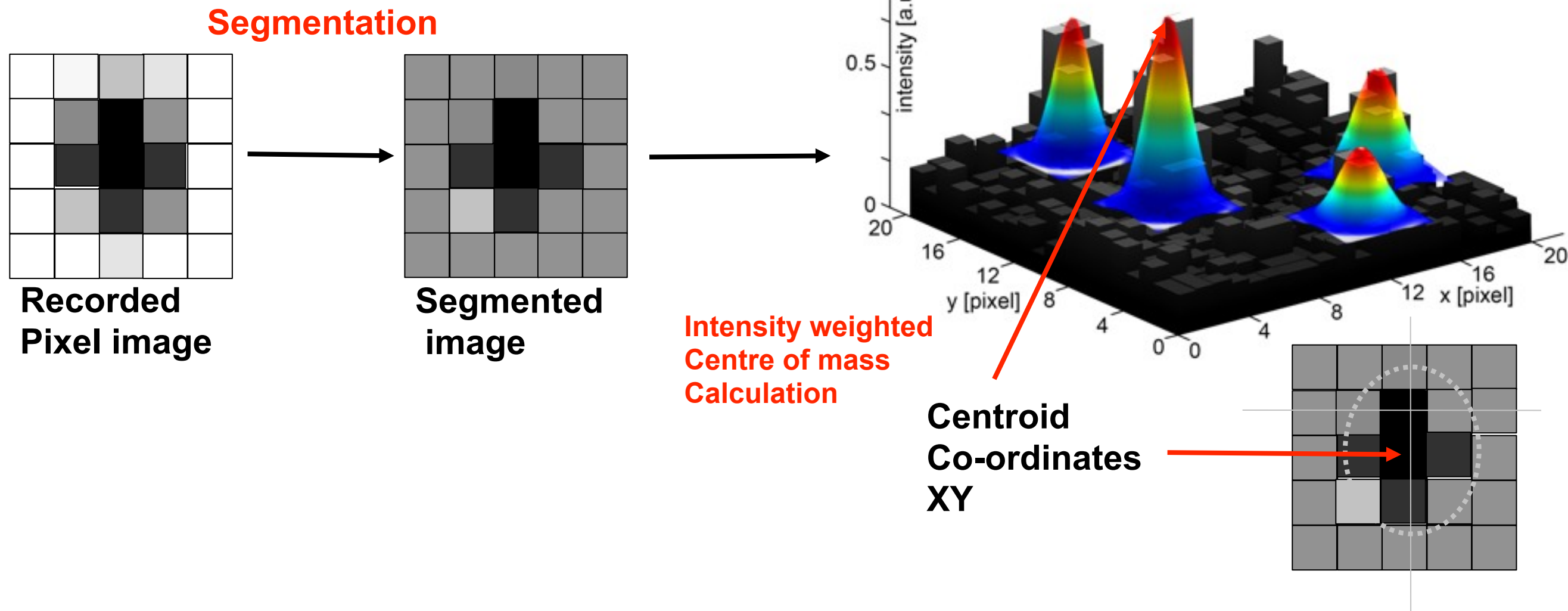


attributes

Intensity segmented **binary** image

Some particles lost - some artificially created

MID LEVEL Processing - centroid



- **Intensity weighted centre of mass** (takes area and intensities into account)
- Output is centroid XY co-ordinates
- **Precision** is greater than the resolution limit
- Seriously limited by **noise**

The human brain is still one of the best segmentation tools

But

Subjective not objective!

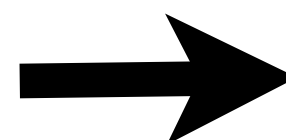
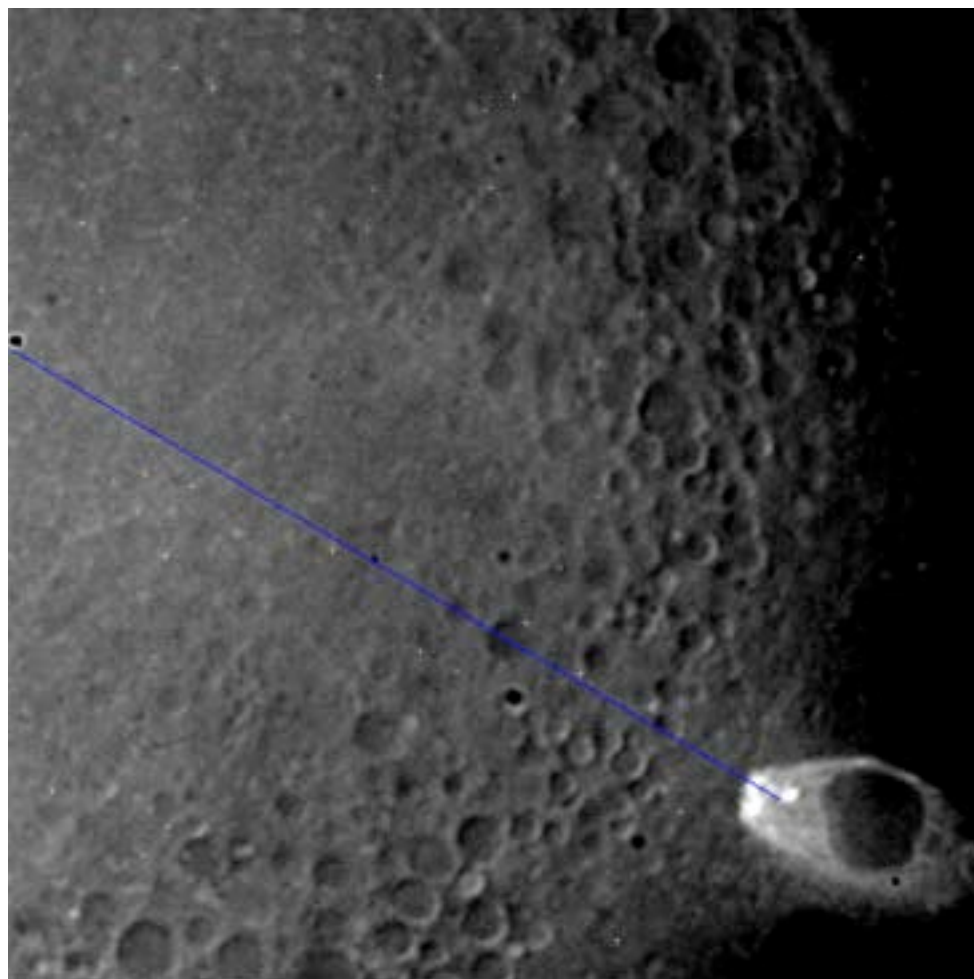


Automated segmentation desirable for **data quality** and **sanity**

HIGH LEVEL Processing

- Outputs are interpretation (making sense)

Automated Particle tracking



Particle velocities

X cent	y cent	dist	Δt	Velocity

Particle trajectories
 Particle velocities
 Run lengths
 Directionality
 Net directionality

Also:

- Ratiometric analysis
- Quantative analysis and Statistics

(See appendices)

Statistical analysis

- Image data requires appropriate statistical analysis:
Experimental design, n-numbers, true independent repeats, numbers
Variation has to be considered within and between images
- May require specialist statistical treatments:
Image values are like percentages, constrained maximum value
Ratio images - skewed distribution of values
Statistics of directionality - “Circular statistics”

Reference Material

Useful sources of Information:

● Confocal List Archive

<http://listserv.acsu.buffalo.edu/cgi-bin/wa?S1=confocal>

● Articles

Rossner & Yamada (2004). What's in a picture? The temptation of image manipulation. *J. Cell Biology* 166: 11–15.

Oberholzer M, et al. (1996). Methods in quantitative image analysis. *Histochem Cell Biol* 105(5): 333-55.

Swedlow et al., (2002). Measuring tubulin content in *Toxoplasma gondii*: A comparison of laser-scanning confocal and wide-field fluorescence microscopy. *PNAS* 99:2014–2019.

● Books

Gonzales & Woods (2002). *Digital Image Processing* 2nd Ed. Prentice-Hall Inc, USA.

Davis, I. (2000). Visualising fluorescence in *Drosophila* - optimal detection in thick specimens. In *Protein Localisation by Fluorescence Microscopy: A Practical Approach*, V. J. Allan, ed. (Oxford, OUP), pp. 131-162.

● General Web Sites

<http://www.microscopyu.com/articles/digitalimaging/index.html>

http://www.cb.uu.se/presentation/baintro/index_eng.html

http://www.olympus-europa.com/medical/39_MicroGlossary.cfm = Jargon buster

http://www.olympus-biosystems.com/downloads/OlympusBioSystems_analySIS_BD.pdf

Processing software

Display

- Adobe Photoshop, MAC/PC
- Jasc Paintshop Pro, PC

Image processing

- NIH ImageJ **FREE**, platform independent
<http://rsb.info.nih.gov/ij/>
<http://www.uhnresearch.ca/facilities/wcif/imagej/> (An ImageJ manual)
<http://www.uhnres.utoronto.ca/facilities/wcif/download.php> (more ImagJ stuff)
- Universal Imaging Metamorph **expensive**, PC
<http://www.universal-imaging.com/products/metamorph/image-analysis.cfm>
- Bitplane (Imaris) **expensive**, PC
http://www.bitplane.com/products/imaris/imaris_product.shtml
<http://www.appliedprecision.com/lifescience/DeltaVisionRT.html>
- Intelligent Imaging Innovations Slidebook **expensive**, PC (incomplete on MAC)
<http://www.intelligent-imaging.com/slidebook/features.php>
- Applied precision **expensive**, Linux (MAC/PC versions = explorer)
<http://www.appliedprecision.com/lifescience/softworxexplorersuite.html>
- Improvision - Velocity, 3D reconstruction **expensive**, (PC, MAC)
<http://www.improvision.com/velocityle>

Additional Topics: further reading

Segmentation

- Gonzales & Woods (2002). Digital Image Processing 2nd Ed. Prentice-Hall Inc, USA.
- <http://www.mia.uni-saarland.de/Research/Segmentation.html>
- http://appsrv.cse.cuhk.edu.hk/~kboxu/research/image_seg.html

3D reconstruction e.g. Improvion - Velocity

- <http://www.improvion.com/velocityle>
- <http://biocomp.stanford.edu/3dreconstructuion/software/index.html>

Movement Tracking

- Tvarusko et al, 2004. Analysing live cell data and tracking Dynamic movements. In Live Cell Imaging a laboratory Manual. Eds RD

Goldman and DL spector. CSHL Press, USA. PP 303-326.

- <http://www.improvion.com/support/tips/Default.lasso?-database=vipoir.FP3&-response=detail.lasso&recID=9&-search>

Ratio imaging

- Parton & Read (1999). Calcium and pH imaging in living cells. In Light Microscopy in Biology - a practical approach 2nd Edition. Ed. A.J. Lacey. Oxford University Press.

Deconvolution

- Parton & Davis (2006). Lifting the fog: image restoration by deconvolution. In Cell Biology Vol 3. Ed. J.E. Celis. Elsevier Press.
- Wallace, W., Schaefer, L.H., Swedlow, J.R. (2001) A workingperson's guide to deconvolution in Light microscopy. BioTechniques 31, 1076-1097.

Wavelets/ Compression

- Gonzales & Woods (2002). Digital Image Processing 2nd Ed. Prentice-Hall Inc, USA.

Additional Topics: further reading

Image archiving/ - Open Microscopy Environment <http://www.openmicroscopy.org/annotation>

Co-localisation / spectral unmixing (an expanding area):

Often provided with multichannel imaging systems

<http://las.perkinelmer.com/content/ApplicationNotes/006914-MembraneTraffickingUsingUltraVIEWRS.pdf>

<http://www.boselec.com/products/documents/FLIMFcorrelationforLSMs4-03.pdf>

http://www.olympus-biosystems.com/downloads/OlympusBioSystems_Spectral_Unmixing.pdf

http://www.olympus.co.uk/medical/22_FV1000_Key_Features.htm

<http://www.olympusfluoview.com/theory/bleedthrough.html>

<http://www.nyas.org/ebriefreps/ebrief/000321/rr/rr06.pdf>

http://www.olympus-biosystems.de/templates_eng/applications/spectral_unmixing.html

Co-localisation with deconvolved data – better XYZ discrimination, 3D modelling

Wiegand U.K., et al. (2003). Red, yellow, green go! - a novel tool for microscopic segregation of secretory vesicle pools according to their age Biochem. Soc. Trans. 31, 851-856.

Alternative to simple colocalisation is FRET (“molecular ruler”)

GU, et al., (2004) Quantitative fluorescence resonance energy transfer (FRET) measurement with acceptor photobleaching and spectral unmixing. *Journal of Microscopy* **215** (2), 162-173.

Additional Topics: further reading

Denoising

<http://www.irisa.fr/vista/Themes/Demos/Debruitage/ImageDenoising.html>

Low level Processing: **Printing - ICC profiles** (for information)

DEFINITION

ICC profile = A file that describes how a particular device reproduces color. The profile defines device gamut in the context of a device-independent color space. International Color Consortium (ICC) = The group established by eight industry vendors (including Adobe Systems) for the purpose of creating, promoting, and encouraging the standardization and evolution of an open, vendor-neutral, cross-platform color management system architecture.

ICC profiles are files that are embedded as part of a document or image. These profiles describe specific information about the image and the output device. These profiles, if used improperly, can cause unwanted color conversions.

ICC profiles are normally embedded by the application saving the PDF, TIFF, or EPS file. To prevent the application you are using from embedding ICC profiles, look closely at the color settings or color management settings for your application. Refer to the application's user manual or online help for more information.

<http://www.color.org/> = ICC colour profile standards

http://www.photoexpert.epson.co.uk/UK/EXPERTISE/how_to_icc_page1.htm (for RGB files)

<http://www.adobe.com/support/downloads/detail.jsp?ftpID=2347> (downloads of Adobe ICC profiles)

<http://www.bodoni.co.uk/profiling/colourprofiling.html#monitor>

Comparing image data

Absolute requirements:

- Systematic image capture parameters
- Systematic image processing and display
- Do the same to experimental and control samples, ideally collect in the same Imaging session

Whenever possible:

- Be systematic in both microscope setup and image capture parameters.
- Image controls in the same imaging session as experimental data.
- Do the same processing and display with your controls as you do to your experimental images.
- - Use internal standards within the experimental design e.g. keep one probe in common.
- - Be very careful directly relating absolute intensity values between image sets, better to compare normalised intensity values. Be aware of the contribution of noise to intensity variation between pixels.
- - Positional information is more easily compared.
-

Swedlow et al., (2002). Measuring tubulin content in *Toxoplasma gondii*: A comparison of laser-scanning confocal and wide-field fluorescence microscopy. PNAS 99:2014–2019.

Co-localisation

- Co-localisation analysis

- Spectral unmixing tools

- Ideal case:

Spectrally distinct markers - no bleed-through / cross talk between channels

Distinct probe localisation - low background

Image **intensities directly proportional to concentrations** of target molecules

Co-localisation of intensities indicates that:

Within the **limits of the optical resolution** - probes occur together

i.e. there are **corresponding sites of local enrichment**

however there is:

no direct evidence of interaction

only **limited direct evidence of stoichiometry**

- Co-localisation and Spectral unmixing software helps to **deal with non-ideal situations** of background and markers which are not spectrally distinct.

- **Using correct image capture / processing** techniques particularly important so not to **misrepresent data**

- Require **controls imaging the single probes** under the same conditions as co-localisation

More details on co-localisation analysis (edited comments from the confocal list)

Co-localisation – more-or-less subjective, difficult to be strictly objective and quantitative.

Therefore it is important to establish valid and stringent criteria and stick to them throughout your experiments. Then you will have a basis to decide if there is more/less/no co-localization in response to treatment. Using automations/software in a mindless manner will not help

Does the finding make biological sense? That is pre-eminent. Conclusions should be supported by more than one method-one should be able to reproduce protein binding and/or immuno-precipitation of the complex.

Merging an essentially 'green' image field with a 'red' one and showing 'yellow' without any detail. Does not represent co-localisation. Specific details must be evident.

Correlation coefficient

Intensity Correlation Analysis from Li et al. Journal of Neuroscience 24, 4070-4081

Based on position and relative intensities: each pixel from the 8-bit image is represented as a pixel on a graph with the x-axis as, for example, 0-256 grey levels for channel 1 (green) y-axis 0-256 grey levels for channel 2 (red). So, a purely red pixel will be placed adjacent to the y-axis, a purely green pixel next to the x-axis, and anything else plotted in between. The assumption is that a pixel plotted near the diagonal where x and y are equivalent represents a point of colocalisation.

Pixel values and photons

- Pixel values relate to photons detected.
- Relating pixel values to photons - requires parameters of the specific detector.

Detector Roper Coolsnap HQ

QE = 62% = only that % of photos is converted to electrons (i.e. detected)

12 bit = 4096 grey levels

Full well depth (6.4 um pixel size) = 12,694 electrons

Pre-Amp gain electrons/ grey scale level = 3.1 (individual camera specific)

Software adds 50 grey scale count offset

-Image signal (300 ms exposure) = 2200 counts (grey level value)

-Dark signal counts (no light) = 150 counts (grey level value) + 50 count offset added

-Signal counts = 2200 - 200 = 2000 3.1 electrons/count = 6200 electrons ~ 6200 photons

- Knowing the number of photons can be important for quantitative image analysis.

Bit Depth / Digitisation

Digitisation

“grey levels” - the **number of discrete values** in an image

the eye detects 6 to 8 bit

Imaging detectors:

8 bit = $2^8 = 256$ grey levels

12 bit = $2^{12} = 4096$ grey levels

16 bit = $2^{16} = 65536$ grey levels